Effects of exhaustive incremental treadmill exercise on diaphragm and quadriceps motor potentials evoked by transcranial magnetic stimulation

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Verin, Eric, Ewen Ross, Alexandre Demoule, Nicholas Hopkinson, Annabel Nickol, Brigitte Fauroux, John Moxham, Thomas Similowski, and Michael I. Polkey. Effects of exhaustive incremental treadmill exercise on diaphragm and quadriceps motor potentials evoked by transcranial magnetic stimulation. J Appl Physiol 96: 253–259, 2004. First published September 5, 2003; 10.1152/japplphysiol.00325.2003—It is unknown whether changes in corticotorcular excitability follow exercise in healthy humans. We hypothesized that a fall in the diaphragm and quadriceps motor-evoked potential (MEP) amplitude elicited by transcranial magnetic stimulation of the motor cortex would occur after an incremental exercise task. In 11 healthy subjects, we measured transdiaphragmatic pressure and isometric quadriceps tension in response to supramaximal peripheral magnetic nerve stimulation. MEPs were recorded from these muscles in response to transcranial magnetic stimulation. After baseline measurements, subjects performed a period of submaximal exercise (gentle walking). Measurements were repeated 5 and 20 min after this. The subjects then exercised on a treadmill with an incremental protocol to exhaustion. Transcranial magnetic stimulation was performed at baseline and at 5, 20, 40, and 60 min after exhaustive exercise, and force measurements were obtained at baseline, 20 min, and 60 min. Mean exercise duration was 18 ± 4 min, and mean maximum heart rate was 172 ± 10 beats/min. Twitch transdiaphragmatic pressure and twitch isometric quadriceps tension were not different from baseline after exercise, but a significant decrease was observed in diaphragm MEP amplitude 5 and 20 min after exercise (60 ± 38 and 45 ± 24%, respectively, of baseline, P = 0.0001). At the same times, the mean quadriceps MEPs were 59 ± 39 and 74 ± 32% of baseline (P < 0.0001 and P < 0.01, respectively). Studies using paired stimuli confirmed a likely intracortical mechanism for this depression. Our data confirm significant depression of both diaphragm and quadriceps MEPs after incremental treadmill exercise.

When striated muscle is excessively loaded, a reversible reduction in efficiency is observed; this phenomenon is termed “fatigue” and may be present, regardless of whether or not a given task can be sustained (6). Although the mechanisms underlying fatigue can be of a peripheral nature (i.e., distal to the neuromuscular junction), central fatigue, better termed supraspinal fatigue, can also occur in humans. The evolution-
Brompton Hospital ethics committee, and all subjects gave their written, informed consent before participation.

**Measurements**

Transdiaphragmatic pressure (Pdi) was measured by using a standard balloon catheter system (catheter length 110 cm; internal diameter 1.6 mm; Ackrad Laboratory, Cranford, NJ) passed through the nose after local anesthesia and placed in the esophagus and stomach to measure esophageal pressure (Pes) and gastric pressure (Pga), respectively. Pes and Pga were measured with linear differential pressure transducers (±100 cmH2O; Validyne, Northridge, CA). Pdi was calculated in real time as Pes − Pga. The Pes, Pga, and Pdi signals were visible to the subjects and the investigators throughout the study.

Quadriceps strength was studied by using a specially designed chair from which the back was removed, on which subjects laid flat with the knee flexed at 90°. Force was measured via an inextensible ankle strap connected to a transducer (Strainstall, Cowes, UK) and carrier amplifier (34).

Surface recordings of the costal diaphragmatic electromyographic activity were obtained by using surface electrodes [bioadhesive neonatal electrocardiogram electrodes (Ag-AgCl), MSB, Ramsbury Marlborough, Wiltshire, UK] placed in the lowest accessible intercostal space between the midclavicular line and the lateral border of the sternum (41). Surface recordings of the quadriceps electromyographic activity were obtained by using surface electrodes [bioadhesive neonatal electrocardiogram electrodes (Ag-AgCl), MSB, Ramsbury Marlborough] placed over the belly of the rectus femoris muscle. The diaphragm and the quadriceps electromyograms were recorded by using a two-channel nerve monitor at 10-kHz sampling rate and 2- to 20-kHz band-pass filtering (Neurosign 100, Magstim, Whitleyland, UK).

**Stimulation techniques.** Phrenic nerve stimulation was achieved by using the bilateral anterior magnetic phrenic stimulation technique (BAMPS) (32). Two Magstim 200 stimulators (Magstim), equipped with 45-mm “figure-of-eight” coils, capable of a maximal output of 2.5 T, were used. All stimulations were delivered in an upright position at the end of a relaxed expiration, as judged by Pes and Pga traces, to control as precisely as possible for the potential confounding effects of lung volume and abdominal configuration on the response to phrenic stimulation (8). Femoral nerve stimulation was achieved unilaterally by using a single stimulator equipped with the same coil as above, according to the previously described technique (34). All peripheral nerve stimuli (both phrenic and femoral nerves) were given at 100% of stimulator output. TMS was achieved by using a single Magstim 200 stimulator equipped with a cone-shaped figure-of-eight coil (maximal output: 2.5 T) positioned over the vertex with handle in the sagittal plane. The head was secured in position by using a head strap. The position of the coil relative to the scalp was optimized in terms of the amplitude of the diaphragm and quadriceps motor potentials evoked in conditions of relaxation with the stimulator output set at 100%. The scalp landmarks were then marked by using an indelible pen to ensure reproducibility of the stimulation conditions throughout the experiments. Subsequently, to standardize the intensity of TMS among subjects, we gave TMS at 20% of output greater than threshold (for the diaphragm). We chose to standardize around the threshold for the diaphragm rather than the quadriceps, because, in pilot studies, we found that this threshold was generally higher than that of the quadriceps. In brief, the method used to establish threshold was that the stimulator output was decreased from 100% by 5% steps until the diaphragmatic response disappeared (present in less than one-half of at least 7 stimuli). The responses of the two muscles to the same TMS shock were studied simultaneously, and the analysis was conducted in each subject, on the dominant side.

**Exercise protocol.** The subjects exercised on a treadmill (Powerjog EG 10, Sports Instruments, Birmingham, UK), according to an incremental design [Bruce protocol (30)]. Transcutaneous oxygen saturation and heart rate were monitored throughout the exercise with a finger probe (Ohmeda Biox 3700, Boulder, CO). The subjects were encouraged to exercise until they reached an intolerable state of dyspnea or exhaustion.

**Experimental Paradigm**

An overview of the experimental paradigm is shown in Fig. 1. Essentially, baseline values were established, and the subjects performed a submaximal exercise task (5-min slow walk in a corridor), which served as a control period. In this study, this exercise was called submaximal exercise. Five and twenty minutes after this, a series of seven TMS was repeated. The incremental exercise test was then performed, and a series of seven TMS was performed 5 min after its end, at 20, 40, and finally at 60 min. BAMS and femoral nerve stimulation were repeated 20 min after the submaximal exercise and 20 and 60 min after the incremental exercise run. At each time point indicated, the mechanical [Tw Pdi and Tw quadriceps force (Q)] and electrical [motor-evoked potential (MEP), elicited by TMS, and the compound muscle action potential (CMAP), elicited by BAMS and femoral nerve stimulation] responses to stimuli were recorded as detailed above.

**Data Analysis and Statistics**

**Conventions for data analysis.** MEP (signal obtained from TMS) or CMAP (signal derived from peripheral nerve stimulation; e.g., femoral nerve stimulation/BAMS) data were retained for analysis when they met the following criteria: 1) absence of gross electrical interference, attested to by a clear return of the EMG signal to baseline after the stimulus artifact and before the muscle response; and 2) absence of contamination from electrocardiographic artifacts. Latencies were measured as the time elapsed between the stimulus and the onset of the action potential, namely, the first departure of the signal from baseline. Amplitudes were measured from peak-to-peak distance of the first potential deflection and expressed in percentage of baseline values. For each of the analysis points, the results of the acceptable responses were normalized against corresponding baseline values. The amplitudes of the Tw Pdi or Q were measured from baseline to peak; Tw Pdi data were only used if they were obtained at end-expiratory lung volume and without swallow artifact, as judged by the Pes trace.

**Statistics.** Statistical analysis was performed by using the StatView 5.0 software (StatView, SAS Institute, Cary, NC) running on an Apple Macintosh computer. We used a one-way analysis of variance with a post hoc protected Fisher’s test. Differences were considered significant when the probability of a type I error was < 0.05. Data in RESULTS are means ± SD.

**Additional Experiments**

**Additional study 1.** In six subjects (three from the original set and three naive ones), the experimental paradigm was reproduced while...
replacing single-shock TMS by paired TMS, according to the procedure originally described by Kujirai et al. (20), in which the first stimulus of the pair acts as a conditioning stimulus. Paired TMS were obtained by using two Magstim 200 stimulators linked by a clocking device set (BiStim, The Magstim, Whitchain, Dyfed, UK) at a 15-ms interstimulus interval that is likely to provoke intracortical facilitation (20). Paired TMS were made at baseline, 5 min after submaximal exercise, and 5, 10, 20, 30, 45, and 60 min after a Bruce protocol exhaustive exercise test. The purpose of this study was to address whether the main observation could be explained by intracortical mechanisms.

Additional study 2. In three subjects from the original set, the experimental paradigm was reproduced (except 20 min after submaximal exercise), with single TMS shock, but using multichannel esophageal diaphragmatic electrodes (Gaeltec, Dunvegan, Isle of Skye, UK) and diaphragmatic surface electrodes. In this additional experiment, the amplitudes were expressed in microvolts. The purpose of this study was to provide independent confirmation that our observations were indeed representative of the diaphragm motor area.

Additional study 3. In three subjects, we tested the variability of MEP amplitude for the costal diaphragm and quadriceps at rest during 1 h. These subjects underwent single TMS shock at baseline and 5, 20, 40, and 60 min after baseline. Amplitudes were expressed in microvolts.

RESULTS

Single TMS and Peripheral Stimulation

Exercise. All of the subjects exercised until exhaustion, with the mean duration of the test being 18 ± 4 min. Their maximum heart rate was 172 ± 10 beats/min, and the transcutaneous oxygen saturation at the end of the exercise was 96 ± 1%.

Responses to phrenic and femoral nerve stimulation. In the 11 subjects, at baseline, mean Tw Pdi was 23.4 ± 5.2 cmH2O, and the mean Tw Q was 12.1 ± 2.6 kg, on average. After exercise, whatever the time, these values were respectively 23.3 ± 5.1 cmH2O and 11.7 ± 4.7 kg (no significant difference), indicating the absence of peripheral contractile fatigue. Three subjects exhibited marked decreases in the amplitude more than of the diaphragm mass action potentials in response to BAMPS, probably because of changes in the recording conditions induced by exercise (for example, changes in skin conductance). The data from these subjects were discarded from analysis of the responses to TMS (Table 1).

Responses to TMS. Both a diaphragm and a quadriceps response to TMS delivered at the maximal stimulator intensity were observed in all subjects. The lowest stimulation intensity at which a diaphragm response was present was 75 ± 10%. The lowest stimulation intensity at which a quadriceps response was present was 50 ± 10% (Table 2).

Figure 2 depicts the evolution of the amplitude of the diaphragm MEP with time. No significant change was induced by the submaximal exercise run, whereas a significant decrease was observed after the maximal exercise run. This decrease was present 5 min after the end of the exercise and reached a nadir at 20 min (respectively, 60 ± 38%, P = 0.0001; 45 ± 24%, P < 0.0001). At 40 and 60 min, the amplitude of the diaphragm MEPs had partly recovered, but remained significantly lower than the baseline value.

As a consequence of this difference in pattern, the reduction in diaphragm MEP amplitude was significantly more marked than the reduction in quadriceps MEP amplitude at 20 min (quadriceps and diaphragm: 74 ± 32 vs. 45 ± 24%; P < 0.001) (Fig. 2).

The average latency of the diaphragm MEP was 17.7 ± 1.0 ms at baseline. There was no significant change after the submaximal exercise run, but it was significantly shorter than...
at baseline 5 min after the real exercise test (17.2 ± 1.1 ms; \( P < 0.05 \)), as well as at 40 and 60 min (17.2 ± 0.9 ms, \( P < 0.01 \) and 17.0 ± 0.8 ms, \( P < 0.0001 \), respectively). The latencies of the quadriceps MEP were unchanged after the submaximal exercise and after the actual exercise.

**Additional Experiments**

**Double TMS: cortical facilitation and inhibition.** A diaphragm and a quadriceps response to paired TMS were observed in all cases and evidenced intracortical facilitation. The evolution with time of the amplitude of the MEP obtained after intracortical facilitation is depicted for the diaphragm and the quadriceps in Fig. 3. The patterns were similar to those observed with single TMS.

**Esophageal diaphragmatic electrode.** The diaphragmatic esophageal electrode recorded shorter MEPs compared with surface electrodes (16.2 ± 0.8 vs. 17.1 ± 1.0 ms, \( P < 0.05 \)) with the same amplitude (220 ± 173 vs. 225 ± 139 \( \mu \text{V} \)). The behavior was the same for the esophageal and the surface electrodes, as illustrated in Fig. 4.

There was a maximum amplitude decrease 20 min after the exercise test (\( P < 0.01 \)) with a beginning of recovery afterward. In these three subjects, there was no change in the MEP amplitudes obtained after peripheral phrenic nerve stimulation.

**Single TMS at rest.** There was no change in diaphragmatic or quadriceps MEPs amplitude over a 60-min period at rest in the three subjects, as shown in Fig. 5. In this experiment, one subject had a low-cortical excitability, which also did not change with time.

**DISCUSSION**

Our data show that the MEPs elicited from the diaphragm and quadriceps muscle by TMS decrease after exhaustive treadmill exercise in healthy humans. Because peripheral contractile fatigue was excluded, this suggests a supraspinal process and generates the hypothesis that central fatigue may have a mechanistic role in task failure. Moreover, comparison of the time course and magnitude of changes in the diaphragm and the quadriceps MEP shows that this process tends to be more pronounced and slower to recover in the diaphragm.

**Methodological Issues**

Two factors are crucial to the validity of our results: the reproducibility of the stimulus and the validity of the chest surface signal as a measure of diaphragm activity.

The position of the stimulating coil in space, the position of the body and of the head of the subjects, and the position of the

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**Fig. 2.** Variations in diaphragm (○) and quadriceps (▲) motor-evoked potentials (MEPs) after submaximal and real exercise, expressed in %baseline, in the 8 subjects studied with single TMS. Quadriceps MEPs were minimal 5 min after the exercise test and then reincreased, whereas diaphragm MEPs continued to decrease 20 min after the end of the exercise test. ns, Not significant. Values are means ± SD. Comparison of diaphragm MEPs or quadriceps MEPs with baseline value: \(* P < 0.05, ** P < 0.01, *** P < 0.001, **** P < 0.001.\) Comparison between diaphragm and quadriceps MEPs: \(§§§ P < 0.01.\)

**Fig. 3.** Variations in diaphragm (D; ○) and quadriceps (Q; ▲) MEPs after submaximal and real exercise, expressed in %baseline, in the 6 subjects studied with paired TMS (15-ms interstimulus interval). Quadriceps MEPs were minimal 5 min after the exercise test and then reincreased, whereas diaphragm MEPs continued to decrease 20 min after the end of the exercise test. Values are means ± SD. Comparison of diaphragm MEPs or quadriceps MEPs with baseline value: \(* P < 0.05, ** P < 0.01, *** P < 0.001.\) Comparison between diaphragm and quadriceps MEPs: \(§§§ P < 0.0001.\)

**Fig. 4.** Variations of esophageal (●) and surface electrode (○) diaphragm MEPs after submaximal and real exercise, in the 3 subjects studied. Esophageal and surface electrodes were well matched and had the same behavior. Values are means ± SD. Comparison of diaphragm MEPs with baseline value: \(* P < 0.05, ** P < 0.01.\)
coil relative to the head were carefully controlled for by the use of ink marks on the scalp and the head strap. The stability of the MEP amplitudes in both the diaphragm and the quadriceps before and after the submaximal exercise makes us confident about our ability to reproduce a reasonably consistent stimulation from one series of measurements to another. Similarly, the stability of CMAP amplitudes in response to peripheral stimulation confirms stability of the recording electrodes for both diaphragm and quadriceps.

Data for study 1 were obtained by using surface electrodes, which record the sum of the activity of the various muscle layers that lie beneath them and are also liable to record activity from distant muscle through volume conduction. TMS cannot specifically activate the cortical area governing the contraction of the diaphragm, and thus the coactivation of several muscles is unavoidable. Therefore, there is a significant risk of signal contamination at the level of chest electrodes, which may complicate the interpretation of changes in MEP. To limit this phenomenon, we placed our “diaphragm” electrodes in a way that has been shown to minimize the risk of signal contamination (9, 41). As a result, in the three subjects in whom surface and esophageal recordings were directly compared, MEPs recorded with esophageal and surface electrodes were well matched in term of latency, tending to be slightly (<1 ms) shorter from the esophageal site, as noted previously by our laboratory and others (22, 29). In these subjects, the effect of exercise on the esophageal and surface-recorded MEP was similar, suggesting that our main data set was indeed recorded from the diaphragm. In addition, an additional argument supports our view that the surface signals are of diaphragmatic origin: specifically, we report depressed rather than increased MEP after exercise. Signal contamination, if present from nonrespiratory muscle, would lead to an underestimation of the extent of the MEP depression. Conversely, if our signals were from extra diaphragmatic respiratory muscle, the finding of exercise-induced MEP depression would still be of scientific interest.

An exercise-induced depression could occur at any site from the cortex to the muscle. Although we believe that we excluded peripheral transmission failure as a cause of our data by measuring the CMAP, our data do not clearly distinguish between various candidate supraspinal sites. However, despite minor protocol differences from the main study, our paired stimulation studies demonstrated a comparable reduction in the facilitated MEP, and this leads us to postulate an intracortical mechanism.

Exercise-induced Contractile Fatigue

The level of pressure developed by the diaphragm in response to BAMPS and the level of force developed by the quadriceps in response to femoral nerve stimulations were not diminished by the exercise protocol performed by the subjects. Regarding the quadriceps, there do not seem to be fatigue data after treadmill exercise in healthy young volunteers, although low-frequency fatigue may be induced by a “stepping exercise” (12) and by cycle exercise (23). For the diaphragm, the occurrence of peripheral low-frequency fatigue after exercise is more controversial. Johnson et al. (19) showed, in 12 healthy volunteers exercising at 85 and 95% of their maximum oxygen uptake, that Tw Pdi was reduced at all lung volumes after task failure. In that study, the contribution of the diaphragm to the respiratory motor output tended to decrease with the duration of the effort, and the authors concluded that “significant diaphragmatic fatigue is caused by the ventilatory requirements imposed by heavy endurance in healthy persons.” These results were confirmed in another study by the same team (1), which also suggested that the mechanism of diaphragm fatigue induced by whole body exercise was a conjunction of blood flow redistribution toward limb muscle reducing diaphragm perfusion and of the diaphragmatic effort. Similarly, Mador et al. (24) also found diaphragm fatigue associated with task failure in sedentary subjects cycling at 80% of their maximal work capacity. However, other data support our premise that diaphragm fatigue is difficult to elicit in healthy subjects; for example, Mador et al. (23) did not find diaphragm fatigue after exhaustive cycling exercise in healthy elderly subjects. Similarly, Levine and Henson (21) found it impossible to elicit low-frequency diaphragm technique in young adults using treadmill exercise alone; indeed, even when an inspiratory resistance was used with treadmill exercise, fatigue was seen in only 5 of 10 subjects. Some of these discrepancies may be due to the difference between cycling and treadmill exercise. In particular, treadmill exercise conducted with the Bruce-type protocol implies a very rapid increase in the effort intensity and may induce dyspnea more intensely and more rapidly than other protocols.

Taken together, these data suggest that task failure associated with contractile diaphragm fatigue during exercise only occurs with the use of very specific protocols rather than as a common occurrence. In our subjects, the combination of an absence of change in diaphragm and quadriceps Tw output with a reduction in the amplitude of the MEP makes it logical to assume that the neuromuscular contribution to task failure, if any, was predominantly central.

Exercise-induced Central Fatigue

A central component to skeletal muscle fatigue can be demonstrated by using the Tw interpolation technique (31) (for review, see Ref. 13). In brief, this technique assesses the degree of voluntary activation of a given muscle by superimposing a supramaximal stimulation of its parent nerve onto voluntary contraction. With this technique, central fatigue has been shown to develop in the quadriceps during sustained maximal voluntary contractions (5) and in other limb muscles (see...
review in Ref. 13). Regarding the diaphragm, it has been shown that the inability of healthy subjects to voluntarily sustain a target Pdi amounting to 75% of the maximal possible value is largely, although not solely, due to a central component of fatigue (4, 28). Guleria et al. (16) have suggested that one explanation for the relative difficulty generating low-frequency fatigue in the diaphragm compared with nonrespiratory muscles could be due to such a phenomenon. Consistent with the present data, that study showed that normal subjects could achieve greater activation of the quadriceps (87.5%) than of the diaphragm (70%) during similar loading protocols and that, consequently, there was a lesser reduction in Tw tension in the diaphragm compared with the quadriceps after the protocol (6 vs. 41%).

Another way to assess central fatigue is to study the response of the muscle of interest to transcranial electrical or magnetic stimulation (see review in Ref. 13). However, the changes in the response to TMS that occur during and after a fatiguing task are complex. During the fatiguing effort itself, both excitatory and inhibitory mechanisms take place. The size of MEP increases (40, 44), and the poststimulation cortical silent period lengths (40). Whereas nonfatiguing tasks induce postexercise facilitation (3, 37), prolonged fatiguing tasks induce postexercise depression (35), although this is not constantly observed (27) and may depend on individual variations of the baseline cortical excitability (44). The depression of the MEP after a fatiguing exercise, first described by Brasil-Neto et al. (7) in the flexor carpi radialis, has been subsequently evidenced in a range of muscles. It can reach 50% of the baseline values, with a variable but progressive recovery of amplitude, which takes place over ≥30 min (7). It is accompanied by a lengthening of the post-TMS silent period (36). The source of the reduction in the corticospinal output is mainly cortical (42), but it may depend on the experimental paradigm. Sacco et al. (36), from the abolition of the postexercise depression in resting MEP by a weak tonic contraction, have shown that decreases in excitability at the spinal level could contribute to the reduced corticomotor excitability that is observed after a fatiguing exercise, such as jogging, 400-m runs induced a marked postexercise depression in MEP without change in peripheral responses to stimulation and without changes in latency. Conversely, predominantly aerobic prolonged exercises, such as jogging, were not associated with postexercise changes in the MEP amplitude. With intense short bouts of exercise-generating high-mechanical forces being a source of muscle damage (11), these observations support the concept of central fatigue as a protective mechanism (13).

**Postexercise Depression of the Diaphragmatic Corticomotor Output**

Our study, by showing postexercise depression of the response to TMS after an exhaustive bout of whole body exercise, is in line with the literature. It is, however, seemingly the first to describe this phenomenon in the diaphragm. We observed a reduced diaphragmatic response not only to single-shock TMS, but also to double-shock TMS performed with a 15-ms interstimulus interval that is known to produce intracortical facilitation in skeletal muscle (20), including the diaphragm (10). Therefore, it is likely that intracortical facilitation of the diaphragm response to TMS was decreased in our subjects, which is an argument in favor of a cortical site for the reduction in the corticomotor output. Excluding subjects with decreased electromyographic responses to phrenic nerve and femoral nerve stimulation from the analysis allows us to rule out a peripheral site. However, we did not use specific approaches to discriminate between a cortical and a spinal site of inhibition (35, 42).

As in other studies, the latency of the quadriceps MEP did not change after exercise in our subjects. This was not the case in the diaphragm, where a reduction in MEP latency was present. This result is surprising, because a shortened diaphragm MEP latency is generally associated with facilitation of the response to TMS (38) rather than with inhibition. However, although sufficiently consistent to reach statistical significance, the shortening in latency was of small magnitude. Hollige et al. (18) observed shortened MEP latencies after whole body exercise of the aerobic type.

The pattern of MEP depression and recovery that we observed in the quadriceps, with an average 35% reduction in size compared with baseline and rapid recovery, resembles that previously observed in hand muscles during focal fatiguing tasks and in limb muscles after whole body exercise (18). In the diaphragm, postexercise depression took longer to reach a nadir than for the quadriceps, reaching a maximum 20 min after the end of exercise, and recovering at a slower pace. There was no major difference in behavior among the subjects, although, anecdotally, the most sedentary among them tended to exhibit an even more marked and more prolonged diaphragmatic depression. The number of subjects involved in this study is, however, too small to allow us to draw any conclusion from this finding, but it would be interesting to test this hypothesis prospectively in larger groups of subjects with different fitness and to study the effects of training on this pattern.

The tendency to observe a more profound and more durable postexercise corticomotor inhibition in the diaphragm than in a locomotor muscle after a “natural” exercise task has various implications. Simply put, this difference could reflect evolutionary development of a tendency for early central diaphragm fatigue, perhaps to protect the organism from overt contractile failure of the diaphragm. This explanation is plausible and would be consistent with early observations that the inspiratory muscles are better able to sustain activity under load (14). However, it ignores the observation that overt diaphragm fatigue does not, even at peak exercise, result in impaired ventilation (19). An alternative explanation is that it is the cortical control of the quadriceps that has undergone evolutionary development to prevent early termination of locomotor tasks, which might include escaping predators or catching animals for food. Study of these and other muscle groups during various tasks relevant to daily life might resolve this issue.

In summary, our data confirm significant depression of both diaphragm and quadriceps MEP after incremental treadmill exercise, suggesting a role for central fatigue in task failure with this protocol. The use of paired stimuli suggests that an
intracortical mechanism is at least partially responsible for this observation. The depression tended to be more pronounced for the diaphragm motor area than the quadriceps motor area, suggesting that regions of the motor cortex have a range of susceptibilities to central fatigue, which may reflect evolutionary-ary pressures.

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REFERENCES


