Lung volumes and respiratory mechanics in elastase-induced emphysema in mice

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1Department of Medical Informatics and Engineering, 2Institute of Surgical Research, University of Szeged, Szeged, Hungary; 3Department of Biomedical Engineering, Boston University, Boston, Massachusetts; and 4Telethon Institute for Child Health Research and Centre for Child Health Research, University of Western Australia, Perth, Australia

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Hantos Z, Adamicza Á, Jánosi TZ, Szabari MV, Tolnai J, Suki B. Lung volumes and respiratory mechanics in elastase-induced emphysema in mice. J Appl Physiol 105: 1864–1872, 2008. First published October 9, 2008; doi:10.1152/japplphysiol.90924.2008.—Absolute lung volumes such as functional residual capacity, residual volume (RV), and total lung capacity (TLC) are used to characterize emphysema in patients, whereas in animal models of emphysema, the mechanical parameters are invariably obtained as a function of transpulmonary pressure (Prs). The aim of the present study was to establish a link between the mechanical parameters including tissue elastance (H) and airway resistance (Raw), and thoracic gas volume (TGV) in addition to Prs in a mouse model of emphysema. Using low-frequency forced oscillations during slow deep inflation, we tracked H and Raw as functions of TGV and Prs in normal mice and mice treated with porcine pancreatic elastase. The presence of emphysema was confirmed by morphometric analysis of histological slices. The treatment resulted in an increase in TGV by 51 and 44% and a decrease in H by 57 and 27%, respectively, at 0 and 20 cmH2O of Prs. The Raw did not differ between the groups at any value of Prs, but it was significantly higher in the treated mice at comparable TGV values. In further groups of mice, tracheal sounds were recorded during inflations from RV to TLC. All lung volumes but RV were significantly elevated in the treated mice, whereas the numbers and size distributions of inspiratory crackles were not different, suggesting that the airways were not affected by the elastase treatment. These findings emphasize the importance of absolute lung volumes and indicate that tissue destruction was not associated with airway dysfunction in this model of mouse emphysema.

EMPHYSEMA IS CLINICALLY CHARACTERIZED by loss of elastic recoil and significant hyperexpansion of the lungs due to a permanent destruction of the parenchymal tissue structure (35). Although a variety of mechanisms including protease-antiprotease imbalance (27), inflammation (23), abnormal extracellular matrix remodeling (46), and mechanical forces (44) have been proposed to be involved in its pathogenesis, the progressive nature of emphysema is still poorly understood (3).

The assessment and evaluation of emphysema raise several questions related to both the functional and structural aspects of the disease. Specifically, the physiological characterization of emphysema requires the measurement of pulmonary or respiratory mechanics (18, 39). In clinical studies, absolute lung volumes such as residual volume (RV), functional residual capacity, or total lung capacity (TLC), as well as their ratios are used to characterize the emphysematous changes (14, 47, 49). To gain insight into the pathogenesis and progression of the human disease, various small animal models of emphysema have been developed (11, 25, 32, 41, 45). However, in animal experiments, the mechanical parameters are most often represented in terms of their dependence on transpulmonary (Pp) or transrespiratory pressure (Prs) or positive end-expiratory pressure (PEEP) (25). This is particularly true for the mouse, the most preferred experimental animal because of the availability of genetic manipulations (12), in which the assessment of changes in absolute lung volume is technically demanding due to the small lung size and is therefore rarely reported. Thus it remains unclear how the physiological findings including the mechanical properties of the lung expressed in terms of Prs or TGV in the various mouse models of emphysema are related to the clinically observable pathophysiological changes in lung volumes and the associated alterations in respiratory resistance and elastance in patients.

The purpose of this study was to establish a link between the mechanical properties of the respiratory system and absolute lung volumes in mice treated with porcine pancreatic elastase (PPE). To this end, we used a previously developed technique to track the elastic and resistive parameters of the respiratory system during slow inspiratory-expiratory maneuvers (19) while recording the changes in lung volume. Our findings suggest that presentation of parameters in terms of absolute lung volumes differ substantially from that in terms of transrespiratory pressures.

METHODS

Animal preparation. Female CBA/Ca mice were anesthetized with an intraperitoneal injection of pentobarbital sodium (75 mg/kg) and intubated with a 20-mm-long, 0.8-mm inner diameter polyethylene cannula under the guidance of a cold light source (model FLQ85E, Helmuth Hund, Wetzlar, Germany), according to the technique described in detail by others (8, 17). The elastase-treated animals received PPE (Sigma-Aldrich Hungary, Budapest, Hungary) in 50 μl of saline in one of two doses: 0.3 IU (n = 15) and 0.6 IU (n = 4) via intratracheal instillation. The control animals (n = 19) received 50 μl of saline only. Three weeks thereafter, the mice were anesthetized with an intraperitoneal injection of pentobarbital sodium (75 mg/kg), tracheotomized, and cannulated with a 0.8-mm inner diameter polyethylene tube. The animals were placed in a custom-built 160-ml body plethysmograph in the supine position and ventilated transmurally with a small-animal respirator (Harvard Apparatus, South Natick, MA) at a rate of 160 min⁻¹, tidal volume of 0.25 ml, and a positive pressure of 10 cmH2O. The costs of publication of this article were defrayed in part by the payment of page charges. The article must therefore be hereby marked “advertisement” in accordance with 18 U.S.C. Section 1734 solely to indicate this fact.

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end-expiratory pressure of 2 cmH2O. Supplemental doses of pentobarbital sodium (15 mg/kg) were administered as needed, generally at the beginning of the measurements. The study protocol was approved by the Institutional Animal Care and Use Committees of the University of Szeged and Boston University.

**Measurement of lung volumes.** Thoracic gas volume (TGV) at end expiration at zero transrespiratory pressure (TGV0) was measured with the plethysmographic technique (13), modified recently for the measurement of thoracic gas volume in anesthetized mice that have weak or no respiratory effort (28). Briefly, 2–3 s after the respirator was stopped, the tracheal cannula was occluded and the intercostal muscles were stimulated via a pair of electrodes arranged diagonally between the upper and lower chest regions, with single impulses of 8–12 V in amplitude and 0.1 ms in duration (model S44, Grass Instruments, Quincy, MA), repeated five to six times in a 10-s recording interval. Figure 1 shows the measurement setup. Plethysmograph pressure ($P_{box}$) and tracheal pressure ($P_{tr}$) were measured with miniature pressure transducers (model 8507C-2, Endevco, San Juan Capistrano, CA), TGV0 was estimated from the $P_{box}$ vs. $P_{tr}$ relationship on the basis of Boyle’s principle, as described previously in detail (28). Following the measurement of TGV0, in 14 control animals (group C1) and 14 elastase-treated mice (group E1) the tracheal cannula was connected to a loudspeaker via a 100-cm, 0.117-cm inner diameter polyethylene tube (a wave tube; see below). After a 5-s pause at end expiration, $P_{box}$ was lowered approximately exponentially to 0 cmH2O by opening the box to atmosphere through a 100-cm, 20-cmH2O, subsequently, $P_{box}$ was lowered to −35 cmH2O through the vacuum line in ~30 s to obtain an estimate of TLC. The box was then opened to atmosphere via a resistor to allow for a passive deflation. This deflation-inflation-deflation maneuver, $V'$ was measured with a capillary bundle (resistance = 180 cmH2O·s·1−1) and the $P_{tr}$ transducer (Fig. 1, inset). Expiratory reserve volume (ERV) was determined by integration, and RV was obtained as TGV0 − ERV.

**Measurement of respiratory impedance.** The tracking estimation of the impedance of the total respiratory system ($Z_{rs}$) during slow inflation-deflation maneuvers was performed in the group C1 and group E1 mice. The measurement of $Z_{rs}$ was similar to that described previously in detail (19), with the modification that a negative body surface pressure was applied (6) instead of the positive pressure inflation. Briefly, $Z_{rs}$ was measured as the load impedance of the wave tube by using a pseudorandom signal between 4 and 38 Hz. Mean $Z_{rs}$ was computed for the first 5 s of oscillation before the inflation started (to estimate $Z_{rs}$ at TGV0) and for every successive 0.5-s interval during the maneuver. Each $Z_{rs}$ spectrum was fitted by a model (20) containing a Newtonian resistance ascribed to the airways (Raw), an inertance (I), and a constant-phase tissue unit characterized by the coefficients of damping (G) and elastance (H). Hysteresis ($\eta$), the ratio of the dissipated and elastically stored energies in the tissue (16), was calculated as $\eta = G/H$. The resistance and the inertance of the tubing including the tracheal cannula were subtracted from Raw and I, respectively; since the inertance of this tubing was the major component of I, the remaining values are considered physiologically unimportant and are not reported.

The slow inflation-deflation maneuvers, together with the preceding measurements of TGV0, were repeated three times in each animal to establish a standard volume history and to ascertain that the Prs-V loops and the $Z_{rs}$ spectra as a function of lung volume were reproducible. The $Z_{rs}$ parameters did not exhibit different volume dependences during inflation and deflation; hence, for clarity, the tracking results are presented only for inflation.

**Crackle sound recordings.** For the measurements in the C2 and E2 groups, the setup was modified so that a microphone ending in a 15-mm-long, 0.7-mm outer diameter metal tube was connected to the tracheal tube adaptor of the plethysmograph (Fig. 1, inset). Tracheal sound was recorded at a sampling rate of 44 kHz and a 16-bit resolution and preprocessed with a GoldWave sound editor (version 5.12, GoldWave, St. John’s NFLD, Canada). High-pass filtering at 2 kHz was used to eliminate the cardiac noise. Subsequently, a short 0.5-ms time window was set up and moved along the sound recording. An individual crackle event was identified if the sound energy in a window increased above a threshold that was chosen to eliminate most of the background noise. The crackle energy was represented by its cumulative distribution defined as the sum of energy up to a given inflation pressure normalized to the total energy, whereas the crackle amplitudes were characterized with their probability density distribution. The details of sound recording and processing are described in Ref. 37.

**Lung morphometry.** At the end of the measurements, the mice were killed with an overdose of pentobarbital sodium, and the heart and the lungs were removed en bloc. The collapsed lungs were then slowly inflated via the tracheal cannula by injecting 1 ml of low melt agarose warmed to 45°C at a concentration of 4%. Successful fixation was accomplished in four elastase-treated and five control mice. Epifluorescence microscopy was employed to study alveolar morphometry in...
two to three slices in each lung. Following thresholding, the alveolar or terminal airspace cross-sectional areas \( A \) were measured using image-processing software (INVIVO, Pictron, Budapest, Hungary), and an equivalent alveolar diameter \( D \) was calculated as \( D = \sqrt{\frac{4A}{\pi}} \). From the values of \( A \), an area-weighted mean equivalent diameter \( D_2 \) was also calculated. The number of \( D \) values obtained in individual animals was not sufficient to compute a complete diameter distribution. Since, by visual inspection, the characteristics of the alveolar structure were similar in the treated animals, we pooled the diameters and constructed single-diameter distribution for both the control and treated mice. The equivalent diameter is useful in that it is not sensitive to shape and it can better characterize the alveolar structure than other morphological indexes in the presence of structural heterogeneity (34).

Statistical analysis. The differences in mechanical parameters between the control and elastase-treated animals were compared using repeated-measures ANOVA tests. The variability of alveolar diameters in each animal was not sufficient to compute a complete diameter distribution. Since, by visual inspection, the characteristics of the alveolar structure were similar in the treated animals, we pooled the diameters and constructed single-diameter distribution for both the control and treated mice. The equivalent diameter is useful in that it is not sensitive to shape and it can better characterize the alveolar structure than other morphological indexes in the presence of structural heterogeneity (34).

RESULTS

Morphometric evaluation of the lung slices (Fig. 2) revealed a significant enlargement of the alveolar airspace sizes in the elastase-treated animals: the equivalent diameter \( D \) increased from 46.5 ± 13.8 \( \mu m \) in the control mice to 70.3 ± 34.2 \( \mu m \) in the treated mice \( (P < 0.001) \). Additionally, the variance of the alveolar diameters was also statistically significantly higher in the treated mice \( (P < 0.001) \). There was a significant increase in the mean area-weighted diameter \( D_2 \) from 55 to 107 \( \mu m \) \( (P < 0.01) \). In both groups, the distribution of the diameters was significantly different from a normal distribution \( (P < 0.001) \). The distribution of diameters was skewed in both groups; however, in the treated mice, the distribution exhibited a significantly longer tail reaching values above 200 \( \mu m \) \( (P < 0.001) \) (Fig. 3).

Elastase treatment resulted in marked and statistically highly significant changes in lung volumes: compared with control, TGV0 and TGV at Prs of 20 cmH2O (TGV20) increased by 52 and 45%, respectively (Table 1). There was no difference between the group E1 mice treated with the 0.3 and 0.6 IU doses of elastase in any of the morphometric indexes or mechanical parameters except \( \eta \) at TGV20 \( (0.170 \pm 0.007 \text{ vs. } 0.157 \pm 0.004; P < 0.01) \). Therefore, both the mechanical and morphometric parameters from the two groups were pooled. The average TGV vs. Prs curves also reflected the changes due to the elastase treatment (Fig. 4), with the mean values of TGV significantly different \( (P < 0.001) \) between the groups at all Prs levels. The ratios of TGV between the groups at the same Prs were fairly constant (between 1.44 and 1.60 for inspiration and between 1.43 and 1.52 for expiration), suggesting a nearly proportional increase of TGV at all Prs, i.e., an unchanged shape of the PV loops. Inspiratory volume (TGV20 − TGV0) increased by 37% in the treated animals, which was also accompanied by a 27% decrease in chord elastance between 0 and 20 cmH2O.

The mechanical parameters obtained from the small-amplitude forced oscillatory measurements of the elastase-treated mice exhibited similarly marked changes: compared with control, the decreases in H were 57 and 27%, respectively, at Prs values of 0 and 20 cmH2O (Table 1). The values of \( \eta \) were also altered by the elastase treatment, with increases more marked at 0 cmH2O (55%) than at 20 cmH2O (12%). By contrast, small and statistically insignificant decreases were observed in Raw at both 0 cmH2O (−2%) and 20 cmH2O (−10%). Since in the inflation-deflation maneuver the pressure protocol was standardized, the group mean values of these parameters were calculated as functions of both Prs and TGV.

Figure 5, A and B, display the dependences of H on Prs and TGV, respectively. The differences in H between group E1 and group C1 animals in the low and high Prs range were in accord with the mean values of H at 0 and 20 cmH2O (see Table 1), whereas this difference disappeared in the pressure range between 9 and 13 cmH2O (Fig. 5A). When plotted as a function of TGV (Fig. 5B), the values of H corresponding to the control and treated animals were completely separated. The mean H at comparable TGV was significantly lower in the treated animals, which suggests that the dynamic elastance in the treated mice reached values similar to those of the control animals at about twice as high absolute lung volumes.

The mean Raw data did not differ between the groups at any value of Prs (Fig. 6A). However, the Raw curves as a function of TGV were remarkably different from those expressed in terms of Prs (Fig. 6B). Elastase treatment resulted in a rightward shift of the mean Raw vs. TGV relationship and, consequently, in statistically significantly higher Raw values at comparable lung volumes (Fig. 6B).

The vital capacity (VC) maneuvers performed in the group C2 and group E2 animals also revealed marked differences in all lung volumes but RV; a typical example is shown in Fig. 7A. The increase in TGV0 in the treated mice
and above 95% within a narrow range of Prs values between 2.5 and 7.5 cmH2O in the treated animals (group C1; n = 14) and the elastase-treated (group E1; n = 14) mice. The cumulative distributions of crackle energy in the two groups of mice (Fig. 7B) as a function of Prs. In group C2, the cumulative energy rises steeply from 0 to above 95% within a narrow range of Prs values between 2.5 and 5 cmH2O. In contrast, the cumulative energy in the E2 group rises almost immediately at the start of inflation but reaches 95% only by a Prs of ~9 cmH2O. Despite the grossly different rates of crackle energy release during inflation, the probability distribution (II) of crackle amplitudes was very similar in the two groups (Fig. 8). Since both distributions followed a linear decrease on a log-log graph, II can be described by a power law as II ~ s^α, where s is the crackle amplitude and α is the exponent of the distribution. Furthermore, α had identical values, close to 2 with a small standard deviation, in the two groups of mice (Fig. 8).

**DISCUSSION**

The primary purpose of this study was to characterize the mechanical properties of the respiratory system in a mouse model of emphysema in terms of Prs and TGV. To achieve this goal, we used a standard elastase treatment protocol and confirmed the presence of emphysema in the treated mice using morphometric analysis of the alveolar structure at a fixed time point, 3 wk following treatment. We also employed a plethysmographic method to determine TGV in mice (28) in combination with a forced oscillation technique that is able to separately estimate the airway and tissue mechanical parameters during slow lung inflation and deflation (19). The main findings of the study are that 1) both the mean and variance of alveolar diameters significantly increased in the treated mice, which resulted in increases in TGV similar to those seen in FRC and TLC in patients with emphysema; 2) dynamic elastance of the lung as a function of Prs was significantly lower in the treated mice except in a narrow range of Prs corresponding to lung volumes approximately halfway between FRC and TLC; 3) when expressed in terms of absolute lung volume, dynamic elastance was markedly lower in the treated mice; and 4) airway resistance (Raw) was significantly higher in the treated group at comparable lung volumes, but the differences disappeared when Raw was plotted as a function of Prs. Furthermore, measurements made in two additional groups of mice revealed that 5) the elastase treatment did not lead to any increase in RV, and the statistics of crackle properties that are related to airway reopening do not substantiate any change in bronchial patency.

**Methodological issues.** Several methodological issues warrant discussion. First, the elastase treatment produces a quick injury-like pathophysiology including the deterioration of lung function and airspace enlargement, whereas human emphysema is usually associated with cigarette smoking with its full development often taking more than 5 years. In this respect, the elastase-induced emphysema does not model the human disease. On the other hand, rodents respond to cigarette smoke in a highly variable manner, and the pathophysiological changes at best mimic mild COPD (48). For the specific purpose of

**Table 1. Thoracic gas volumes and oscillatory mechanical parameters**

<table>
<thead>
<tr>
<th>Group</th>
<th>Weight, g</th>
<th>TGV0, ml</th>
<th>TGV20, ml</th>
<th>H0, cmH2O/ml</th>
<th>H20, cmH2O/ml</th>
<th>η0</th>
<th>η20</th>
<th>Raw0, cmH2O·s·ml⁻¹</th>
<th>Raw20, cmH2O·s·ml⁻¹</th>
</tr>
</thead>
<tbody>
<tr>
<td>CI</td>
<td>29±2</td>
<td>0.31±0.06</td>
<td>0.76±0.11</td>
<td>52±10</td>
<td>129±9</td>
<td>0.24±0.02</td>
<td>0.15±0.01</td>
<td>0.46±0.14</td>
<td>0.12±0.02</td>
</tr>
<tr>
<td>E1</td>
<td>29±3</td>
<td>0.47±0.10</td>
<td>1.10±0.18</td>
<td>22±7</td>
<td>94±12</td>
<td>0.38±0.07</td>
<td>0.17±0.01</td>
<td>0.45±0.18</td>
<td>0.11±0.02</td>
</tr>
</tbody>
</table>

Values are means ± SD. Thoracic gas volumes (TGV) and oscillatory mechanical parameters are at transrespiratory pressures of 0 cmH2O (suffix 0) and 20 cmH2O (suffix 20) in the control (group CI; n = 14) and the elastase-treated (group E1; n = 14) mice. H, elastance coefficient; η, hysteresitivity; Raw, airway resistance; NS, statistically not significant.

![Graph showing TGV vs. Prs](image-url)
comparing lung physiology as expressed in terms of absolute lung volume or transrespiratory pressure, the widely used elastase treatment targeting the tissue compartment is appropriate. Second, it has been reported that there exists a second "knee" in the pressure-volume curve of mice beyond 20 cmH₂O (42). To avoid the rapid changes in mechanical properties of such a second knee, the tracking maneuvers were limited to a maximum inflation pressure of 20 cmH₂O. We note, however, that the inflation curves initiated from RV (groups C2 and E2) followed a single sigmoidal and were reproducible, and hence we defined TLC as the value of TGV reached at Prs = 35 cmH₂O, while acknowledging the problems of the definition of TLC in mice (42). Another issue is related to the measurement of the quasi-static and dynamic properties of the total respiratory system. The contribution of the chest wall to the total respiratory elastance is small in mice, which implies a negligible impact on the pressure-volume curve (30) and a <10% share in the dynamic elastance (25, 40). Therefore, any change in H following elastase treatment must be proportional to alterations in lung tissue properties. We should also note that, although the parameter Raw estimated from the model fitting to the Zrs data represents not only airway resistance but all frequency-independent (Newtonian) viscous losses in the respiratory system, the contribution of the chest wall to the Newtonian resistance was shown to be negligible at any lung volume in mice (40).

Parenchymal structural changes. It has recently been shown that the trapped gas volume in excised lungs from a variety of animal models of emphysema correlated with morphometric evaluation of the alveolar structure (29). In the present study, the larger absolute gas volumes in the treated animals were also associated with a significant increase in the equivalent diameters (D) of the airspaces. It is interesting to note that, in response to elastase treatment, the mean D increased by 51%, which is close to the 45% increase in TGV. Furthermore, the equivalent diameters were not normally distributed (Fig. 3), and the treatment resulted in a significant stretch of the tail of the diameter distribution from ~100 to 200 μm. As a consequence, the standard deviation of the equivalent diameters nearly tripled, whereas the mean area-weighted diameter D₂ doubled following treatment. Since both the variance and D₂ are sensitive to heterogeneities (34), these results imply that the elastase treatment significantly increased the structural hetero-

Fig. 5. A: elastance coefficient (H) vs. transrespiratory pressure (Prs) during slow inflation from Prs of 0–20 cmH₂O. The values in each animal were averaged for successive 2.5-cmH₂O ranges of Prs. The mean values of H for the animals in the control (group C1) mice (●) and the elastase-treated (group E1) mice (○) are statistically significantly different (P < 0.05) at Prs of <8 cmH₂O and Prs of >14 cmH₂O. Bars denote standard deviation. B: H vs. thoracic gas volume (TGV). The values of H are statistically significantly different between the two groups at all ranges of Prs (P < 0.05).

Fig. 6. A: airway resistance (Raw) vs. transrespiratory pressure (Prs) during slow inflation from Prs of 0–20 cmH₂O. The values in each animal were averaged for successive 2.5-cmH₂O ranges of Prs. No statistically significant difference was found between the mean values of Raw for the control (group C1) mice (●) and the elastase-treated (group E1) mice (○) in any range of Prs. Bars denote standard deviation. B: Raw vs. thoracic gas volume (TGV). The values of Raw are statistically significantly different between the two groups for all TGV (P < 0.05).
The increased heterogeneity is also supported by the fact that the coefficient of variation of diameters increased from 30% in control to 49% in the treated mice.

The increase in heterogeneity is consistent with the possibility that the enzymatically weakened alveolar walls rupture under the influence of mechanical forces (44). The presence of elastase in the interstitium not only leads to digestion of the elastin of the connective tissue, but it also triggers complex cellular repair processes (46). Such repair is likely abnormal (46), and the corresponding extracellular assembly of collagen results in mechanically weak collagen fibers in the alveolar walls. At points of stress concentration, the weak collagen and the alveolar wall break. Following rupture, the stress is redistributed in the neighborhood, and, consequently, the nearby intact regions start to experience new stress concentration (39). This ongoing process necessarily leads to an increase in structural heterogeneity as well as a progressive decrease in lung recoil. The latter in turn results in a larger TGV at the same Prs in the treated mice (Fig. 4).

Dynamic tissue properties. Although H decreased significantly in the treated mice both at low and high Prs (Table 1), the initial decrease in H with increasing Prs and the reversal toward higher Prs values remained a characteristic feature of the H vs. Prs relationship following the elastase treatment (Fig. 5A). However, the initial decrease reverses at a lower Prs in the elastase-treated mice, and this is in accordance with the results of a study on mice spontaneously developing emphysema (tight skin mice) and their controls, in which lung elastance was measured as a function of PEEP (24). The elevation in H at high Prs is likely due to the stretching of the respiratory tissues and recruiting collagen in the lung parenchyma (19, 40), whereas the mechanisms behind the initial decrease in H are less clear: they may include alveolar recruitment, reorganization of the tissue matrix and the surfactant layer (19, 25, 40), or chest wall mechanics (22). Whatever the mechanism, the biphasic pattern of the H vs. Prs is also seen as a function of TGV and is not altered by the elastase treatment (Fig. 5B);

![Figure 7](image1.png)

**Fig. 7.** A: thoracic gas volume (TGV) vs. transrespiratory pressure (Prs) curves recorded during vital capacity maneuvers in a control (group C2) and an elastase-treated (group E2) mouse. Arrows indicate the bottom knees of the inflation curve. B: cumulated crackle sound energy $\Sigma E$ normalized by its maximum value ($\Sigma E_{\text{max}}$) in the control and the treated mice. Pooled data are in both groups.

Table 2. *End-expiratory thoracic gas volume, residual volume, vital capacity, and total lung capacity*

<table>
<thead>
<tr>
<th>Group</th>
<th>Weight, g</th>
<th>TGV0, ml</th>
<th>RV, ml</th>
<th>VC, ml</th>
<th>TLC, ml</th>
<th>$P_{\text{tknee}}$, cmH$_2$O</th>
<th>$N_c$/infl</th>
</tr>
</thead>
<tbody>
<tr>
<td>C2</td>
<td>33±2</td>
<td>0.32±0.09</td>
<td>0.20±0.10</td>
<td>1.28±0.26</td>
<td>1.48±0.20</td>
<td>21.5±1.0</td>
<td>148±111</td>
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<tr>
<td>E2</td>
<td>33±2</td>
<td>0.49±0.08</td>
<td>0.15±0.03</td>
<td>1.95±0.18</td>
<td>2.10±0.19</td>
<td>15.9±1.3</td>
<td>166±72</td>
</tr>
<tr>
<td>P</td>
<td>NS</td>
<td>&lt;0.02</td>
<td>NS</td>
<td>&lt;0.001</td>
<td>&lt;0.001</td>
<td>&lt;0.001</td>
<td>NS</td>
</tr>
</tbody>
</table>

Values are means ± SD. End-expiratory thoracic gas volume (TGV0), residual volume (RV), vital capacity (VC), total lung capacity (TLC) corresponding to the transrespiratory pressure of 35 cmH$_2$O, pressure at the bottom knee of the thoracic gas volume vs. transrespiratory pressure curve ($P_{\text{tknee}}$), and the number of crackles during an inflation maneuver ($N_c$/infl) in the control (group C2; $n = 5$) and the elastase-treated mice (group E2; $n = 5$).

J Appl Physiol • VOL 105 • DECEMBER 2008 • www.jap.org
nevertheless, when H is plotted against TGV, the separation between the two groups becomes more apparent.

Tissue hysteresivity was also markedly affected by the elastase treatment. The 55% increase in \( \eta \) at end-expiration is in accord with several previous studies (7, 25, 31). Brewer et al. (7) argued that the increased \( \eta \) is a result of remodeling of the alveolar walls. At higher lung volume, the difference between the values of \( \eta \) of the two groups, both exhibiting a significant fall from the values obtained at end-expiration, was drastically reduced to 12%. The decrease in \( \eta \) with increasing lung volume has been attributed to the increasing contribution of collagen to tissue resistance (15, 40). Additionally, Ito et al. (26) reported that, following elastase treatment of mice, respiratory elastance decreased despite a nearly 50% increase in the total collagen content of the lung, implying an abnormality in collagen function. Together with the increase in tissue heterogeneity discussed above, the abnormal collagen function might also have contributed to the overall increase in \( \eta \) in the treated mice (Table 1).

Airway resistance and structure. Several studies using animal models of emphysema have pointed out that the tissue destruction manifested in elevations in TGV and decreases in elastance are not associated with increased airway or pulmonary resistance (2, 4, 5, 9, 33), and some observations on human emphysema also indicate that airspace enlargement and airflow limitation do not necessarily combine (10, 38, 47). In this context, the changes following elastase treatment observed in the present study may characterize an initial or mild degree of emphysema where the loss of alveolar attachments, which must have accompanied the marked increase in both alveolar size and lung volumes, is compensated by new elastic equilibria within the lung parenchyma itself as well as between the lung and chest wall so that the patency of the airways is retained. Therefore, we paid particular attention to the possible alterations in airway function and established that the average Raw vs. Prs relationships of the control and treated groups were remarkably similar (Fig. 6A). Another indicator of the intact airway function was the lack of any increase in airway collapsibility during forced expiration to RV, the only lung volume that, quite unexpectedly, did not change in this emphysematous group. In contrast, since a weakened parenchymal tethering, which characterizes the E2 group, reduces the probability of reopening airways (36), one might expect that the opening pressures would actually be higher in the E2 group. In fact, by examining the cumulative distributions in Fig. 7B, both of these statements are true. Indeed, on the one hand, the difference in cumulative crackle energy does imply that some airways must be more difficult to open in the E2 group since 95% of the total energy is reached only at Prs of 9 cmH\(_2\)O compared with Prs of ~5 cmH\(_2\)O in the C2 group. On the other hand, there are crackles that are triggered at a much lower Prs in the E2 than in the C2 group, indicating that some airways open very easily in the former. Although the reduced tethering in the E2 group explains why some airways are more difficult to open in the E2 group, we are unsure about the exact mechanism responsible for the reduction in airway opening pressures following treatment. Assuming that surface tension is not altered by the elastase treatment, we can speculate as follows. Computer simulations mimicking the breakdown of lung parenchyma have shown that, when the breakdown is governed by mechanical forces, a significant heterogeneity develops in the network (44). This leads to a wide distribution of mechanical forces around the damaged area, including elastic elements that carry significantly smaller as well as larger forces than before the breakdown (24). The higher forces would then generate locally an increased tethering and hence a reduced opening pressure. Nevertheless, the above uncertainties indicate that further
investigations involving time course studies with a longer time period after the elastase treatment are warranted to further characterize the relevance of this murine model of emphysema to the human disease.

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