Muscle fiber size and function in elderly humans: a longitudinal study

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THE LOSS OF MUSCLE MASS (sarcopenia) and strength in elderly is one of the most significant physiological and clinical problems in gerontology and geriatrics. The incidence of sarcopenia increases with advancing age and is not limited by geographic region or ethnic group (4). In older men and women, muscle weakness and atrophy are causally related to the loss of functional independence, increase in morbidity, higher rate of hospitalization, and mortality after bone fractures due to falls (26). In the elbow and knee extensors and flexors of aging humans, the loss of muscle strength ranges from 1 to 3% per year (13). In the vastus lateralis, this strength loss could partly be explained by a 1% reduction per year in the number of muscle fibers (23).

Several studies have reported age-related decrements in muscle size and function at the whole muscle level (8, 9, 13). However, the loss is neither universal nor homogeneous. It is noteworthy that, in one longitudinal study, approximately one-third of the participating individuals (mean age at start of study = 60.4 yr) showed no loss of muscle strength over 10 yr (15). We have reported significant differences in specific force in single skinned muscle fibers between young and older men (10). In that study, however, there were no significant differences in muscle fiber cross-sectional area, and the reduction in specific force was due to a reduction in maximal single fiber force generation. This lack of muscle atrophy was also noted using histochemical techniques in a longitudinal study of nine older men, suggesting that surviving muscle fibers may compensate by maintaining their size (8).

Sarcopenia has been studied using both cross-sectional and longitudinal research designs. Cross-sectional studies are likely to underestimate the losses and represent a comparison only with those that have survived advanced age. In other words, persons with stronger muscles may have a better chance of being included in cross-sectional studies because they have survived to old age. The true magnitude and nature of the loss of muscle size and function in older men and women can only be determined in longitudinal studies of the same cohort of individuals. The fact that these types of studies are difficult to carry out may explain the limited longitudinal data in the scientific literature. To our knowledge, no study has looked at changes in single muscle fiber contractility and muscle quality (force adjusted by fiber size) in a longitudinal fashion. Further, no longitudinal study has combined whole muscle and single fiber experiments in the same cohort of individuals. The purpose of the present investigation was to examine changes in whole muscle and single fiber size and function in a cohort of aging humans over ~9 yr.

MATERIALS AND METHODS

Subjects. Twenty-four subjects (12 men) completed the study protocol in 1997–1998 (T1) including knee extensor strength testing, computed tomography (CT) scans of the thigh, and biopsies of the vastus lateralis muscle. In 2005–2006 (T2), attempts were made to contact all 24 prior participants. Four had died, two moved away, two subjects could not be located to send recruitment materials, and four subjects were contacted by mail and phone but elected not to participate. The remaining 12 subjects (5 men) enrolled and completed the study. All 12 subjects completed strength testing and CT scans of the thigh. For two subjects we did not have the CT data for 1997–1998 and thus the comparison is limited to 10 subjects (Table 1). Nine subjects were significantly lower at follow-up. This was accompanied by a...
were reconstructed on a 512-manner using SliceOmatic v4.2 software (Montreal, Canada). Images of 1s
m of the femur for each subject. The length of the femur was

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included). AT areas were measured in the range of

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analysis was consulted as a guide. Muscle CSA was measured in the

muscle and normal-density muscle CSA (areas of AT not

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From the images, the cross sectional areas (CSAs) for normal density

previously reported (9). The placement of the lever arm with relation
to the subject’s leg was carefully controlled. The subjects performed

bex II, Medway, MA) was used to measure strength (N

CT. A CT scan of the nondominant thigh was performed at the
midpoint of the femur for each subject. The length of the femur was
determined from a coronal scout image as the distance between the
intercondylar notch and the trochanteric notch. At T1, the scanner was a
GE Highspeed Advantage CT scanner (Milwaukee, WI) operating at
100 kV and 170 mA. Scans were obtained at T2 using a Siemens
Somatom Scanner (Erlangen, Germany) operating at 120 kV and 100
mA. Technical factors were slice width of 10 mm and a scanning time
of 1 s.

All scans were analyzed by a single investigator in a blinded
manner using SliceOmatic v4.2 software (Montreal, Canada). Images
were reconstructed on a 512 × 512 matrix with a 25-cm field of view.
From the images, the cross sectional areas (CSAs) for normal density
muscle and low density muscle, subcutaneous adipose tissue (AT),
subfascial AT, and intramuscular AT were measured using manual
tracing. A one-pixel width line was used to separate anterior from
posterior muscle groups, using, when applicable, intramuscular AT as
a guide. To ensure proper placement of this line on T2 scans, the T1
analysis was consulted as a guide. Muscle CSA was measured in the
range of 0-100 Hounsfield units (HU) and calculated as the sum of
low-density muscle and normal-density muscle CSA (areas of AT not
included). AT areas were measured in the range of −190 to −30 HU.
One tracing was drawn between, on the inside edge of the fascia, to
distinguish between subcutaneous AT and subfascial AT. Similarly,

another tracing was drawn to separate subfascial AT from intramus-
cular AT, defining subfascial AT as that lying just below the fascial
plane. Intermuscular AT was defined as AT lying between and among
muscle groups. These methods have been previously described (12, 16).

Whole muscle specific force. For each of the muscle compartments,
whole muscle specific force was calculated as the ratio of muscle
strength and muscle CSA.

Muscle biopsy. Muscle biopsies were taken from the vastus lateralis
muscle at the level of the CT scan using a 5-mm Dacron biopsy
needle (3) and suction (6). The same biopsy site was used on each
occasion (T1 and T2) since it was possible to identify the scar of the
biopsy at T1 in all subjects.

The specimen was divided in two pieces. One piece was laid down
longitudinally in a plastic cryomold, mounted in embedding medium
(OCT, Sakura Finetek, Torrance, CA), frozen in isopentane slush,
cooled to the temperature of liquid nitrogen, and stored in liquid
nitrogen for later sectioning and staining.

For histochemical analysis, serial 10-μm cross sections were cut in
a cryostat (Leica CM1850) at −24°C. To obtain values of fiber-type
mean area, sections were stained for myofibrillar ATPase at pH 9.40
after preincubation at pH 4.35. The mean number of fibers counted per
biopsy was 69 ± 26 (range 32-107) in T1 and 442 ± 229 (range
56–716) in T2. Measurements of type I and II fiber areas were
performed using the NIH Image-based software Scion Image for
Windows (Scion, version alpha 4.0.3.2). All measurements were done
once for calculation of muscle fiber areas. Only areas without artifacts
and distinct cell borders were measured. The mean number of fibers
measured per biopsy was 33 ± 9 (range 17–40) in T1 and 228 ± 133
(range 12–421) in T2.

Single muscle fiber experiments. The second piece of the biopsy
was placed in relaxing solution (see below) at 4°C within 1-2 min of
being obtained. Bundles of ~30 fiber segments were dissected free
from the samples and then tied with surgical silk to glass capillary
tubes at slightly stretched lengths. The fiber segments were chemically
skinned for 24 h in relaxing solution containing 50% (vol/vol) glyc-
erol at 4°C and were subsequently stored at −20°C for up to 4 wk
before use.

A detailed explanation of the general methods used in this study
has been published by others (20). Briefly, on the day of an experi-
ment, fiber segments were placed for 30 min in relaxing solution
containing 0.5% Brij-58 (polyoxethylene 20 cetyl ether; Sigma, St.
Louis, MO) before mounting in an experimental apparatus, similar to
that described previously (25). A fiber segment length of 1-2 mm was

subjects underwent muscle biopsies, and the other three were ex-
cluded because of concurrent coumadin therapy.

The volunteers received a complete explanation of the purposes
and procedures and gave their written consent. A comprehensive
medical evaluation, including a medical history, physical examina-
tion, routine blood and urine tests, and a resting electrocardiogram,
was performed before their participation in the study at both time
points. The level of recreational activity and sports participation over
the last year was estimated using a questionnaire (22). This study was
approved by the Human Investigation Review Committees of Tufts
University-Tufts Medical Center and Spaulding Rehabilitation Hos-
pital.

Muscle strength measurements. An isokinetic dynamometer (Cy-
bex II, Medway, MA) was used to measure strength (N·m) of the
nondominant knee extensors and flexors at 60°/s and 240°/s, as
previously reported (9). The placement of the lever arm with relation
wart to the subject’s leg was carefully controlled. The subjects performed
five maximal voluntary contractions at each velocity, and the peak

was placed in relaxing solution (see below) at 4°C within 1-2 min of
the experiment. Needle biopsies were performed on the day of the
experiment, providing muscle samples for the study. In addition,
a biopsy was performed on each occasion (T1 and T2) since it was
possible to identify the scar of the previous biopsy at T1 in all subjects.

The specimen was divided in two pieces. One piece was laid down
longitudinally in a plastic cryomold, mounted in embedding medium
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Table 1. General characteristics of subjects (n = 12)

<table>
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<tr>
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<tr>
<td>Age, yr</td>
<td>71.1±5.4</td>
<td>80.0±5.3</td>
</tr>
<tr>
<td>Body weight, kg</td>
<td>71.2±7.7</td>
<td>72.6±10.4</td>
</tr>
<tr>
<td>Height, m</td>
<td>1.67±0.1</td>
<td>1.65±0.1</td>
</tr>
<tr>
<td>Body mass index, kg/m²</td>
<td>25.8±2.8</td>
<td>26.6±3.2</td>
</tr>
<tr>
<td>Duration of follow-up, yr</td>
<td>8.9±0.7</td>
<td>8.9±0.7</td>
</tr>
<tr>
<td>Physical activity index, kcal/wk</td>
<td>2.9±1.63</td>
<td>2.2±1.62</td>
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</table>

Values are mean ± SD with minimum and maximum values in parentheses.

<table>
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<tbody>
<tr>
<td>Knee extensors 60°/s</td>
<td>98.5±27.4</td>
<td>76.3±23.4</td>
</tr>
<tr>
<td>Knee flexors 60°/s</td>
<td>56.7±16.9</td>
<td>59.5±18.9</td>
</tr>
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</table>

Table 2. Longitudinal changes in isokinetic muscle strength (N·m) of the nondominant leg (n = 12)

| Knee extensors 60°/s | 98.5±27.4 | 76.3±23.4 | <0.001 |
| Knee flexors 60°/s | 56.7±16.9 | 59.5±18.9 | 0.38  |

Values are means ± SD.
left exposed to the solution between connectors leading to a force transducer (model 400A; Aurora Scientific, Aurora, Ontario, Canada) and a DC torque motor (model 308B; Aurora Scientific). The apparatus was mounted on the stage of an inverted microscope (Olympus IX70, Tokyo, Japan). While the fiber segments were in relaxing solution, sarcomere length (SL) was set to 2.75-2.85 \( \mu m \) by adjusting the overall segment length (10).

The sarcomere length, the segment diameter, and the length of segment between the connectors were measured with an image analysis system (Image-Pro Plus, Media Cybernetics, Silver Spring, MD). Fiber diameter was measured by recording the vertical displacement of the microscope nosepiece while focusing on the top and bottom surfaces of the fiber. The focusing control of the microscope was used as a micrometer. In our hands the coefficient of variation for three measurements done by the same observer is 0.5% for diameter and 3.7% for depth. Fiber cross-sectional area was calculated from the diameter and depth, assuming an elliptical circumference. Maximum force (Po) was adjusted for fiber cross-sectional area after adjusting diameter and depth, assuming an elliptical circumference. Maximum force (Po) was adjusted for fiber cross-sectional area after adjusting fiber area for the 20% swelling that is known to occur during skinning (11, 25).

Relaxing and activating solutions (in mM) 4 MgATP, 1 free Mg\(^{2+}\), 20 imidazole, 7 EGTA, 14.5 creatine phosphate, and KCl to adjust the ionic strength to 180 mM. The pH was adjusted to 7.0. The concentrations of free Ca\(^{2+}\) were \(10^{-9}\) M (relaxing solution) and \(10^{-4.5}\) M (maximum activating solution) and are expressed as pCa (\(-\log [Ca^{2+}]\)). Apparent stability constants for Ca\(^{2+}\)-EGTA were corrected for temperature (15°C) and ionic strength (180 mM) (7). A computer program (7) was used to calculate the concentrations of each metal, ligand, and metal-ligand complex.

Immediately preceding each activation, the fiber was immersed for 10–20 s in a solution with a reduced Ca\(^{2+}\)-EGTA buffering capacity. This solution was identical to the relaxing solution except that EGTA was reduced to 0.5 mM, which resulted in a faster attainment of steady tension during subsequent activation. Maximum active force (Po) was calculated as the difference between the total force in activating solution (pCa 4.5) and the resting tension measured in the same segment while in the relaxing solution. All contracture measurements were carried out at 15°C. Fibers with visible tears and fibers demonstrating a loss of force >10% of the baseline value were not used for the analysis.

### Maximal unloaded shortening velocity

Maximal unloaded shortening velocity was measured using the slack test (5).

### Myosin heavy chain composition

After mechanical measurements, each fiber was placed in SDS sample buffer in a plastic microfuge tube and stored at \(-20^\circ C\) for up to 1 wk or at \(-80^\circ C\) if the gels were to be run later. The myosin heavy chain (MyHC) composition of single fibers was determined by SDS-PAGE (19). The acrylamide concentration was 4% (wt/vol) in the stacking gel and 6% in the running gel, and the gel matrix included 30% glycerol. Sample loads were kept small (equivalent to ~0.05 mm of fiber segment) to improve the resolution of the MyHC bands (types I, IIA, IIB). The conditions in which the SDS-PAGE were run include constant current (24 mA) for 5.5 h. Proteins were identified using a combination of human myosins from vastus lateralis muscles and from reports in the literature (20).

### Table 3. Longitudinal changes in specific peak torque (N·m/cm²) of the nondominant leg (n = 10)

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<tbody>
<tr>
<td>60°/s</td>
<td>2.15±0.3</td>
<td>1.73±0.3</td>
<td>-0.42 ±0.2</td>
<td>-19.3±7.7</td>
<td>-2.2±1</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>240°/s</td>
<td>1.23±0.3</td>
<td>0.83±0.3</td>
<td>-0.40 ±0.2</td>
<td>-32.9±12.2</td>
<td>-3.7±1.3</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Knee flexors</td>
<td>60°/s</td>
<td>1.08±0.2</td>
<td>0.08±0.3</td>
<td>8.4±24</td>
<td>1.03±2.8</td>
<td>0.34</td>
</tr>
<tr>
<td></td>
<td>240°/s</td>
<td>0.7±0.23</td>
<td>-0.05±0.2</td>
<td>-4.9±20</td>
<td>-0.54±2.3</td>
<td>0.29</td>
</tr>
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</table>

Values are means ± SD.

### Statistical analysis

All variables were examined for normality both graphically and statistically. Means and SDs were calculated. Paired samples t-tests and Wilcoxon matched pairs signed-rank tests were used to detect significant differences between T1 and T2. Statistical significance was accepted if the two-tailed P value was <0.05. Data were analyzed using SPSS statistical software (version 15.0 for Windows, Chicago, IL).

### RESULTS

#### Subjects

The characteristics of the subjects are presented in Table 1. After 8.9 yr of follow up, the subjects were older, but body weight, body mass index, and the physical activity index had not changed significantly.

#### Muscle strength

Significant losses in muscle strength of the knee extensors were noted at slow and fast angular velocities (Tables 2 and 3; Figs. 1 and 2). The average percent loss per year was 2.56 at 60 °/s and 4.20 at 240°/s. No significant changes were noted in the knee flexors. Whole muscle specific force was lower in the knee extensors but did not change in the knee flexors.

#### Thigh composition

A significant reduction in total muscle cross-sectional area (4.5%) and total anterior muscle area (5.7%) was observed (Table 4). The posterior muscle group did not change.

#### Histochemical analysis of muscle fiber composition and size

No changes were noted at T2 in fiber type distribution (Table 5 and Fig. 3). No significant changes were seen in average fiber area.

#### Size and contractile properties of single muscle fibers

A total of 411 fibers were studied (247 at T1). At T2, type I fibers showed no change in diameter (\(P = 0.16\)) or cross-sectional area (\(P = 0.80\)) (Table 6). Type IIA fibers had a larger (\(P = 0.02\)) diameter at T2 and a nonsignificant increase (\(P = 0.17\)) in cross-sectional area. A trend toward an increase (\(P = 0.07\))

![Fig. 1. Longitudinal changes in isokinetic knee extensor muscle strength. T1: 1997–1998, T2: 2005–2006. Values are means ± SD. *P < 0.001.](http://jap.physiology.org/10.2203.32.2.on July 7, 2017)
in maximal force was noted in both type I and IIa fibers. Specific force showed the same trend ($P = 0.07$) only in type I fibers. Maximum unloaded shortening velocity was unchanged in either fiber type.

**DISCUSSION**

To our knowledge, this is the first study of longitudinal changes in whole muscle and single muscle fiber contractile properties in the same cohort of elderly subjects. The main observations of the present longitudinal study are 1) a significant loss of maximal knee extensor muscle force; 2) a significant reduction in whole muscle area, particularly of the anterior compartment of the thigh; 3) no change in fiber-type distribution or mean type I and II fiber area; 4) a significant increase in type IIa fiber diameter; and 5) no decrease in single fiber maximal force or specific force in both fiber types. Of particular interest is the contrast between the changes at the whole muscle level vs. the microscopic level. While in vivo muscle strength and whole muscle size showed the expected age-associated losses, the analysis of cross sections stained with histochemical techniques and the experiments performed with permeabilized single fibers suggest that individual muscle fibers that survived the effects of aging compensated for the loss of motor units by maintaining size, force production, and single fiber quality.

**Whole muscle size and function.** The rate of loss of strength of the knee extensors found in the present study compares favorably with a recent three year follow-up of a large cohort of 1,880 volunteers with a mean age of 73.5 yr (13). These investigators reported annualized losses of knee extensor muscle strength of 2.6 to 4.1%. The losses were higher in men than women. Our present longitudinal findings showed larger reductions in muscle strength of the knee extensors expressed as percent change per year than our previous cross-sectional studies (9): 2.5 and 4.2 vs. 1.8 and 1.1 at slow and fast angular velocities, respectively. In general, these observations confirm our earlier findings of greater rates of muscle strength decline when the same cohort of subjects is measured longitudinally compared with cross-sectional differences among various age groups (15). When similar testing methods are used, this difference between studies of different designs is most likely due to selection bias of healthy older subjects in cross-sectional studies. Persons with stronger muscles may have a better chance of being included in cross-sectional studies because they have survived to old age.

A significant difference between the present study and previous longitudinal investigations (8, 15) is the fact that, in the present study, the flexors of the knee maintained their strength at follow-up at both slow and fast angular velocities. An explanation for this discrepancy is not immediately obvious. Some muscles may be more susceptible to the effects of aging than others. For example, in women, the loss of strength in the elbow extensors and flexors is less than the loss of strength in the knee extensors and flexors (15). In addition to possible intrinsic muscle susceptibility, several factors such as the level of limb-specific physical activity and the presence of diseases with regional effects (i.e., knee osteoarthritis) may also contribute to larger losses in some muscle groups.

It has been argued that the age-related decline in muscle strength is partially due to the loss of muscle mass (8, 13). In the present study, the pattern of muscle atrophy is similar to that of the loss of strength. In other words, the reduction in total muscle cross-sectional area can be explained by losses in the anterior (extensor) compartment of the thigh while no changes were observed in the posterior (flexor) compartment. Thus the absence of muscle loss in the flexor compartment may have contributed to the preservation of the strength of the flexor muscle group. It is interesting that the absolute and relative losses in the anterior compartment in the present study are smaller than in our previous study (8). This may be due to the fact that the subjects in the present study were older and had a smaller muscle size at baseline. Another possibility is that they

Table 4. **Skeletal muscle and thigh adipose tissue area (n = 10)**

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<tbody>
<tr>
<td>Total area, cm$^2$</td>
<td>186.5±45.0</td>
<td>173.8±35.2</td>
<td>−13.2±24</td>
<td>−6.3±9</td>
<td>0.06</td>
</tr>
<tr>
<td>Total muscle area, cm$^2$</td>
<td>98.3±21.8</td>
<td>92.9±15.4</td>
<td>−5.4±8</td>
<td>−4.5±6</td>
<td>0.03</td>
</tr>
<tr>
<td>Total subcutaneous adipose tissue, cm$^2$</td>
<td>80.8±46</td>
<td>69.9±39</td>
<td>−9.2±21</td>
<td>−9.2±16</td>
<td>0.17</td>
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<tr>
<td>Anterior muscle groups</td>
<td></td>
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<tr>
<td>Total muscle, cm$^2$</td>
<td>45.9±8.1</td>
<td>43.2±8</td>
<td>−2.7±2.2</td>
<td>−5.7±4.5</td>
<td>0.005</td>
</tr>
<tr>
<td>Subfascial adipose tissue, cm$^2$</td>
<td>0.91±0.4</td>
<td>0.77±0.3</td>
<td>−0.14±0.3</td>
<td>−12.7±23</td>
<td>0.11</td>
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<tr>
<td>Intramuscular adipose tissue, cm$^2$</td>
<td>0.54±0.3</td>
<td>0.73±0.5</td>
<td>0.2±0.6</td>
<td>58.8±102</td>
<td>0.20</td>
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<tr>
<td>Posterior muscle groups</td>
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<tr>
<td>Total muscle, cm$^2$</td>
<td>52.4±14.7</td>
<td>49.7±9.2</td>
<td>−2.7±7</td>
<td>−3.2±9</td>
<td>0.20</td>
</tr>
<tr>
<td>Subfascial adipose tissue, cm$^2$</td>
<td>3.1±1.6</td>
<td>3.37±2.0</td>
<td>0.31±0.99</td>
<td>16.2±46</td>
<td>0.34</td>
</tr>
<tr>
<td>Intramuscular adipose tissue, cm$^2$</td>
<td>2.9±1.3</td>
<td>2.7±1.5</td>
<td>0.25±1.2</td>
<td>−6.2±32</td>
<td>0.33</td>
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</table>

Values are mean ± SD.
Table 5. Longitudinal changes in muscle fiber type and area (n = 8)

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<tr>
<td>Distribution, %</td>
<td></td>
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<tr>
<td>Type I</td>
<td>38.8 ± 13</td>
<td>38.5 ± 21</td>
<td>−0.39 ± 15</td>
<td>−2.1 ± 35</td>
<td>0.94</td>
</tr>
<tr>
<td>Type II</td>
<td>61.2 ± 13</td>
<td>61.6 ± 21</td>
<td>0.39 ± 15</td>
<td>−0.3 ± 27</td>
<td>0.94</td>
</tr>
<tr>
<td>Area, μm²</td>
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<td></td>
</tr>
<tr>
<td>Type I average area</td>
<td>4,069 ± 1,080</td>
<td>4,524 ± 1,324</td>
<td>455 ± 1,275</td>
<td>13.98 ± 30</td>
<td>0.35</td>
</tr>
<tr>
<td>Type II average area</td>
<td>3,649 ± 1,056</td>
<td>3,664 ± 1,213</td>
<td>15 ± 1,818</td>
<td>9.2 ± 37.6</td>
<td>0.67</td>
</tr>
</tbody>
</table>

Values are mean ± SD.

maintained a similar level of physical activity during the period of observation (Table 1).

Muscle fiber type distribution and size. As shown in Fig. 3, histochemical analysis of muscle cross sections stained for myofibrillar ATPase demonstrated no changes in muscle fiber-type distribution. This is in contrast with our previous longitudinal report (8) of a reduction in percentage of type I fibers after 12 yr. However, in that study, the volunteers were younger at baseline (mean age 65 yr). Also, the percentage of type I fibers at follow-up (40%) was very similar to the 38% reported at baseline and follow-up in the present study. The differences between studies may also be due to the inherent variability in fiber-type distribution in various areas of the vastus lateralis and the limitations of the muscle biopsy technique. On the other hand, in both the present and our previous study, no statistically significant change in mean cross-sectional area in either fiber type was observed. In fact, in the present study, a nonsignificant trend (P = 0.35) was in the direction of an increase in average type I fiber area. The lack of statistical significance may be related to a relatively small number of subjects and/or fibers and the possibility of a type II error.

Experiments with permeabilized single muscle fibers. We are reporting for the first time longitudinal changes in permeabilized single muscle fibers obtained with the percutaneous muscle biopsy technique. Of importance, both type I and IIA fibers showed no atrophy after 10 yr using diameter or cross-sectional area as indexes of fiber size. In fact, the diameter of type IIA fibers was significantly larger (P = 0.02) at follow-up although the fiber cross-sectional area was not significantly larger. This mismatch between changes in diameter and cross-sectional area could be explained by flattening of the fibers that has been reported to be more pronounced among type II fibers (2).

Maximal force production at the single fiber level tended to be higher (P = 0.07) at follow-up in both type I and IIA fibers. Because type I fiber size did not change, specific force (an index of muscle quality) also tended to be higher (P = 0.07) at follow-up. In the case of type IIA fibers, specific force did not change.

These data differ from a cross-sectional study published by our group (10). A cross-sectional comparison of young and older groups with an average difference in age of 37 yr demonstrated significantly lower maximal force and specific force in type I and IIA fibers in elderly. The inclusion of healthier older survivors in the present study could explain these differences between studies. Another possible explanation is that the subjects in the present study were more physically active and maintained their weekly caloric expenditure over the 10 yr. In addition, a time span of 9 yr may have been too short to detect a significant change in contractile function in the very old, and the relatively small number of subjects increases the possibility of a type II statistical error.

Compensatory muscle hypertrophy. Compensatory hypertrophy in animal models is a well-known phenomenon that occurs after, for example, selective tenotomy of agonist muscles. The presence of atrophied and hypertrophied fibers has been reported in late middle-aged rat soleus muscle (14). Finally, a mutation of the gene for IIB myosin heavy chain that leads to the loss of muscle fibers results in compensatory hypertrophy of all fiber types in the mouse (1). Therefore, different pathological and age-related conditions can be associated with compensatory hypertrophy. In humans, this phenomenon has been described and documented using magnetic resonance imaging at the whole muscle level after selective neurectomy (21).

Table 6. Longitudinal changes in single muscle fiber size and contractile properties (n = 9)

<table>
<thead>
<tr>
<th></th>
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</tr>
</thead>
<tbody>
<tr>
<td>Type I</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>No. of fibers</td>
<td>183</td>
<td>105</td>
<td>0.16</td>
</tr>
<tr>
<td>Diameter, μm</td>
<td>92 ± 13</td>
<td>100 ± 13</td>
<td>0.80</td>
</tr>
<tr>
<td>Cross-sectional area, μm²</td>
<td>5020 ± 1140</td>
<td>4910 ± 1190</td>
<td>0.07</td>
</tr>
<tr>
<td>Maximal force, μN</td>
<td>493 ± 108</td>
<td>605 ± 191</td>
<td>0.72</td>
</tr>
<tr>
<td>Specific force, N/cm</td>
<td>14.8 ± 2.0</td>
<td>19 ± 5.7</td>
<td>0.07</td>
</tr>
<tr>
<td>Shortening velocity, fiber length/s</td>
<td>0.75 ± 0.12</td>
<td>0.73 ± 0.17</td>
<td>0.72</td>
</tr>
<tr>
<td>Type IIA</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>No. of fibers</td>
<td>64</td>
<td>59</td>
<td>0.02</td>
</tr>
<tr>
<td>Diameter, μm</td>
<td>83 ± 6</td>
<td>101 ± 16</td>
<td>0.17</td>
</tr>
<tr>
<td>Cross-sectional area, μm²</td>
<td>4,230 ± 530</td>
<td>4,840 ± 1,260</td>
<td>0.88</td>
</tr>
<tr>
<td>Maximal force, μN</td>
<td>482 ± 113</td>
<td>541 ± 168</td>
<td>0.07</td>
</tr>
<tr>
<td>Specific force, N/cm</td>
<td>17 ± 3.5</td>
<td>17 ± 5.0</td>
<td>0.88</td>
</tr>
<tr>
<td>Shortening velocity, fiber length/s</td>
<td>1.54 ± 0.25</td>
<td>1.26 ± 0.32</td>
<td>0.13</td>
</tr>
</tbody>
</table>

Values are means ± SD.
Selective neurectomy of the nerve to the medial gastrocnemius resulted in atrophy of the medial gastrocnemius and compensatory hypertrophy of the lateral gastrocnemius and part of the soleus muscle. A similar lesion of the nerve to the soleus resulted in hypertrophy of the gastrocnemius muscle. However, in that study, the evaluation of muscle size was limited to whole muscle and muscle fibers were not studied.

It is possible that some of the age-associated changes in skeletal muscle are induced by disuse. Thus it may seem contradictory to find no change in muscle size or strength in single fibers obtained from aged muscle. It could be that the relative maintenance of levels of physical activity in the present study had a preventative effect. However, other human models of prolonged disuse showed similar findings. The absence of atrophy and weakness in single muscle fibers after prolonged disuse has been reported in patients with chronic spinal cord injury (SCI) (24), amyotrophic lateral sclerosis (18), and inclusion body myositis (17). Patients with chronic SCI, both complete and incomplete, demonstrated nonsignificant increases in cross-sectional area and maximal force of type I and IIa single fibers compared with normal control subjects. The authors speculated that the main effect of chronically reduced neuromuscular activity is a loss of muscle cells, leaving a population of surviving fibers that have equal or better contractile performance. Similar to the findings in our study, this preservation of size and contractile performance was not dependent on the fiber type.

Our findings suggest that sarcopenia should not be conceptualized as a linear process that begins after 30 yr of age and progresses at a constant rate beyond age 80 yr. The loss of muscle mass with advancing age may be more like a hyperbola with a slower rate of muscle loss in older age groups partially due to compensatory single muscle fiber hypertrophy or maintenance of muscle fiber size. These findings suggest a dissociation between changes in muscle size and the process that results in the loss of muscle strength.

Conclusion. We report longitudinal changes in whole muscle size and strength in older adults that is consistent with previous reports. We also show for the first time that despite these changes at the whole muscle level, single muscle fiber contractile function is preserved with advancing age. These data suggest that with loss in whole muscle size, existing fibers that have survived may compensate to partially correct these deficits in an attempt to maintain optimal force-generating capacity even at very old age (80 yr).

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