Control of heart rate variability by cardiac parasympathetic nerve activity during voluntary static exercise in humans with tetraplegia

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Takahashi M, Matsukawa K, Nakamoto T, Tsuchimochi H, Sakaguchi A, Kawaguchi K, Onari K. Control of heart rate variability by cardiac parasympathetic nerve activity during voluntary static exercise in humans with tetraplegia. J Appl Physiol 103: 1669–1677, 2007. First published August 30, 2007; doi:10.1152/japplphysiol.00503.2007.—Heart rate (HR) is controlled solely by cardiac parasympathetic outflow in tetraplegic individuals, who lack supraspinal control of sympathetic outflows and circulating catecholamines but have intact vagal pathways. A high-frequency component (HF; at 0.15–0.40 Hz) of the power spectrum of HR variability and its relative value against total power (HF/Total) were assessed using a wavelet transform to identify cardiac parasympathetic outflow. The relative contribution of cardiac parasympathetic and sympathetic outflows to controlling HR was estimated by comparing the HF/Total-HR relationship between age-matched tetraplegic and normal men. Six tetraplegic men with complete cervical spinal cord injury performed static arm exercise at 35% of the maximal voluntary contraction until exhaustion. Although resting cardiac output and arterial blood pressure were lower in tetraplegic than normal subjects, HR, HF, and HF/Total were not statistically different between the two groups. When tetraplegic subjects developed the same force during exercise as normal subjects, HF and HF/Total decreased to 67–90% of the preexercise control and gradually recovered 1.5 min after exercise. The amount and time course of the changes in HF/Total during and after exercise coincided well between both groups. In contrast, the increase in HR at the start of exercise was blunted in tetraplegic compared with normal subjects, and the HR recovery following exercise was also delayed. It is likely that, although the withdrawal response of cardiac parasympathetic outflow is preserved in tetraplegic subjects, sympathetic decentralization impairs the rapid acceleration of HR at the onset of exercise and the rapid deceleration following exercise.

Heart rate (HR) is controlled solely by cardiac parasympathetic nerve activity during voluntary static exercise in humans with tetraplegia. J Appl Physiol 103: 1669–1677, 2007. First published August 30, 2007; doi:10.1152/japplphysiol.00503.2007.—Heart rate (HR) is controlled solely by cardiac parasympathetic outflow in tetraplegic individuals, who lack supraspinal control of sympathetic outflows and circulating catecholamines but have intact vagal pathways. A high-frequency component (HF; at 0.15–0.40 Hz) of the power spectrum of HR variability and its relative value against total power (HF/Total) were assessed using a wavelet transform to identify cardiac parasympathetic outflow. The relative contribution of cardiac parasympathetic and sympathetic outflows to controlling HR was estimated by comparing the HF/Total-HR relationship between age-matched tetraplegic and normal men. Six tetraplegic men with complete cervical spinal cord injury performed static arm exercise at 35% of the maximal voluntary contraction until exhaustion. Although resting cardiac output and arterial blood pressure were lower in tetraplegic than normal subjects, HR, HF, and HF/Total were not statistically different between the two groups. When tetraplegic subjects developed the same force during exercise as normal subjects, HF and HF/Total decreased to 67–90% of the preexercise control and gradually recovered 1.5 min after exercise. The amount and time course of the changes in HF/Total during and after exercise coincided well between both groups. In contrast, the increase in HR at the start of exercise was blunted in tetraplegic compared with normal subjects, and the HR recovery following exercise was also delayed. It is likely that, although the withdrawal response of cardiac parasympathetic outflow is preserved in tetraplegic subjects, sympathetic decentralization impairs the rapid acceleration of HR at the onset of exercise and the rapid deceleration following exercise.

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0.15–0.40 Hz mainly reflects cardiac parasympathetic outflow, whereas the low-frequency (LF) component of HRV at 0.04–0.15 Hz has a more complex relation with cardiac sympathetic and parasympathetic nerve activity (33). The present study was undertaken 1) to identify the changes in CVNA from the HF component of HRV in tetraplegic and normal subjects and 2) to examine a relative contribution of CVNA and CSNA to cardiac autonomic control of HR by assessing the relationship between HR and the HF component.

METHODS

Subjects. Six men with tetraplegia (age, 35.7 ± 3.2 yr) and nine age-matched normal subjects (age, 33.8 ± 2.2 yr) participated in this study; body weight and height of the tetraplegic subjects were 53 ± 2.2 kg and 172 ± 2.3 cm, respectively; body weight and height of the normal subjects were 70 ± 2.3 kg and 173 ± 2.2 cm, respectively. All subjects had neither cardiopulmonary disease nor medications likely to affect the results of the present study. The tetraplegic subjects, who had complete traumatic spinal cord injury at the cervical spinal level of C6 or C7, had no detectable somatic motor and sensory function at and below the level of lesion (American Spinal Injury Association grade A). Their postinjury period ranged from 7 to 22 yr. They were able to tolerate upright sitting posture in a wheelchair and to perform physical activities in daily life such as mobility, transfers (bed to chair and back), and dressing etc. They regularly participated in sports activities of wheelchair basketball and/or tennis for ∼1.5 h once a week. This study was performed in accordance with the Declaration of Helsinki and approved by the Institutional Ethics Committee. The experimental protocols and procedures were well explained to them in advance and informed consent was obtained from all participants. A part of the results in the present study was obtained by reanalyzing our laboratory’s previous data (31).

Experimental protocols. Static contraction of the right elbow flexors was performed with the subjects in the supine position on a comfortable bed. The tetraplegic subjects were asked to empty the bladder before starting the experiments, to avoid possible bladder discomfort during exercise, because upper arm cuff pressure would disturb static contraction of the right elbow flexors. The beat-to-beat values of stroke volume (SV), cardiac output (CO), and total peripheral resistance (TPR) were simultaneously calculated with a Modelflow software (BeatScope 1.1, Finapres Medical Systems). The Modelflow method used a nonlinear three-element model of aortic input impedance to compute aortic blood flow from the arterial pressure waveform (39). The noninvasive method has been considered to provide the same group-averaged value of CO during exercise, compared with CO determined by CO2 or acetylene rebreathing (25, 32), Doppler ultrasound (30), or pulse dye densitometry (18).

Power spectral analysis. We analyzed the power spectrum of HRV from pulse interval using the Wavelet transform of a Flucllet system (Dainippon Pharmaceutical, Osaka, Japan), which had a high time resolution power of 1 s and allowed examination of the instantaneous changes in autonomic control of cardiac excitation rhythm (20). The absolute power density of the LF and HF spectral components was determined as the mean value every successive 1 s. We also calculated the normalized unit of the LF and HF spectral components [denoted LF/Total and HF/Total, respectively] by dividing the absolute power of each spectral component by the total power in the range of 0.04–2.0 Hz and multiplying this value by 100. The normalization procedure is helpful in allowing comparisons among the subjects or the experimental conditions characterized by a difference in total power (23, 33).

Data and statistical analyses. Because the endurance period differed among the subjects, the cardiovascular variables and the power spectral parameters obtained from HRV were aligned either at the start of or at the end of voluntary static exercise and then averaged sequentially over a period of 10 s. The cardiovascular and HRV responses during and after exercise were expressed as the relative changes against the control values during the preexercise period for 1 min. When we examined using a Kolmogorov-Smirnov test whether all data obtained in this study were distributed normally, all variables showed normal distribution. They were analyzed using a one-way ANOVA with repeated measures in each of the normal and tetraplegic groups. The statistical level of significance was defined as P < 0.05. The data are expressed as means ± SE.

RESULTS

Workload and endurance period. The absolute and relative workload of static elbow flexion was the same between the normal and tetraplegic groups. The endurance period until exhaustion was also similar between the two groups (normal 167 ± 11 s vs. tetraplegic 162 ± 17 s). The results suggested that tetraplegic subjects showed similar motor performance and time to fatigue as normal subjects.

Cardiovascular responses to static exercise. The baseline cardiovascular values are summarized in Table 1. The baseline MAP was significantly lower by 34% in tetraplegic compared with normal subjects. The baseline CO was lower by 19% in tetraplegic compared with normal subjects, although cardiac index was not different (tetraplegic 3.1 l·min⁻¹·m⁻² vs. normal 3.4 l·min⁻¹·m⁻²). TPR also tended to be lower by 19% in tetraplegic subjects, although the difference was not statistically different. On the other hand, the baseline values of HR,
pulsatile interval, and SV were not different between the two groups. The decreased CO and TPR contributed to the hypotension in tetraplegic subjects.

A typical example of the beat-to-beat changes in HR, MAP, SV, CO, and TPR throughout the experiment in one subject of each group is shown in Fig. 1. The time course of the changes in HR, pulsatile interval, and MAP during static exercise are compared between the normal and tetraplegic groups in Fig. 2. The peak values of the cardiovascular parameters during static exercise are summarized in Table 1. In normal subjects, HR abruptly increased at the onset of static exercise as exemplified in Fig. 1. The initial increase in HR of 9 ± 2 beats/min was significant at 10 s from the exercise onset, which was followed by a gradual increase until the end of exercise (Fig. 2). In contrast, the increase in HR was not significant in tetraplegic subjects until 40 s from the exercise onset (Figs. 1 and 2). However, the peak increase in HR at the end of exercise was similar between the two groups (normal 17 ± 2 beats/min vs. tetraplegic 20 ± 4 beats/min). Following exercise, the recovery of HR in tetraplegic subjects was slower than that in normal subjects (Fig. 2). Like HR, the decrease in pulse interval at the onset of exercise and the recovery of pulse interval after exercise were blunted in tetraplegic subjects compared with normal subjects (Fig. 2). Like HR, the decrease in pulse interval at the onset of exercise was slower than that in normal subjects. Following exercise, the HF component showed the opposite responses between the two groups; the HF component tended to increase transiently above the preexercise control level in normal subjects, whereas the HF component gradually returned toward the control in tetraplegic subjects (Fig. 3). On the other hand, the HF/Total component gradually returned to the control ~90 s after the end of exercise, with the same time course in both groups.

The LF and LF/Total components decreased during static exercise in both groups (Fig. 3). It was interesting that the time course and magnitude of the relative decreases in the HF and HF/Total components during exercise well coincided between the two groups (Fig. 3); the peak decrease in the HF component was 71 ± 7% in normal subjects and 73 ± 9% in tetraplegic subjects (Fig. 4, Table 1). The peak decrease of 90 ± 4% in the HF/Total component tended to be greater in tetraplegic subjects than that of 67 ± 11% in normal subjects. Following exercise, the HF component showed a gradual decrease during exercise in both groups (Fig. 3). There was a significant difference in the peak change in the HF/Total component between the two groups (Fig. 4). Following exercise, the LF component showed a large increase in normal subjects, whereas the LF component in tetraplegic subjects and the LF/Total component in both normal and tetraplegic subjects returned to the control without such a surge.

**Relationship between the HF/Total component and HR.** To evaluate the relative contribution of cardiac sympathetic and parasympathetic outflows to autonomic control of HR in the intact condition, the relationship between the relative changes in the HF/Total component (as an index of CVNA) and HR are compared between normal and tetraplegic subjects in scattered diagrams of Fig. 5. The slope of the gross linear relationship between the changes in the HF/Total component and HR

Table 1. Baseline cardiovascular values and their responses during and after exercise in normal and tetraplegic subjects

<table>
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<tr>
<th></th>
<th>Normal Men (n = 9)</th>
<th>Tetraplegic Men (n = 6)</th>
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<tr>
<td></td>
<td>Before</td>
<td>Peak Value During Exercise</td>
</tr>
<tr>
<td>HF, ms⁻²</td>
<td>99 ± 26</td>
<td>28 ± 13*</td>
</tr>
<tr>
<td>LF, ms⁻²</td>
<td>75 ± 20</td>
<td>150 ± 106*</td>
</tr>
<tr>
<td>HR/Total, %</td>
<td>13 ± 1</td>
<td>4 ± 1*</td>
</tr>
<tr>
<td>LF/Total, %</td>
<td>10 ± 1</td>
<td>16 ± 2.5</td>
</tr>
<tr>
<td>HR, beats/min</td>
<td>68 ± 3</td>
<td>84 ± 3*</td>
</tr>
<tr>
<td>Pulse interval, ms</td>
<td>912 ± 35</td>
<td>720 ± 28*</td>
</tr>
<tr>
<td>MAP, mmHg</td>
<td>95 ± 6</td>
<td>125 ± 5*</td>
</tr>
<tr>
<td>SV, ml</td>
<td>94 ± 6</td>
<td>79 ± 4*</td>
</tr>
<tr>
<td>CO, l/min</td>
<td>6.3 ± 0.3</td>
<td>7.0 ± 0.4*</td>
</tr>
<tr>
<td>TPR, MU</td>
<td>0.95 ± 0.10</td>
<td>1.18 ± 0.12*</td>
</tr>
<tr>
<td></td>
<td>205 ± 108</td>
<td>21 ± 8</td>
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<tr>
<td></td>
<td>115 ± 58</td>
<td>18 ± 7</td>
</tr>
<tr>
<td></td>
<td>15 ± 2</td>
<td>1.2 ± 1*</td>
</tr>
<tr>
<td></td>
<td>12 ± 2</td>
<td>1.3 ± 3†</td>
</tr>
<tr>
<td></td>
<td>61 ± 4</td>
<td>82 ± 6*†</td>
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<tr>
<td></td>
<td>1,018 ± 80</td>
<td>777 ± 68*†</td>
</tr>
<tr>
<td></td>
<td>63 ± 2†</td>
<td>76 ± 5*†</td>
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<tr>
<td></td>
<td>87 ± 11</td>
<td>73 ± 11*</td>
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<tr>
<td></td>
<td>5 ± 1.4†</td>
<td>5.9 ± 0.5*</td>
</tr>
<tr>
<td></td>
<td>0.77 ± 0.07</td>
<td>0.82 ± 0.09†</td>
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Values are means ± SE. HF, a high-frequency power between 0.04 and 0.15 Hz; LF, a low-frequency power between 0.15 and 0.4 Hz; Total, a total power between 0.04 and 2.0 Hz; HR, heart rate; MAP, mean arterial blood pressure; SV, stroke volume; CO, cardiac output; TPR, total peripheral resistance; MU, medical unit (= mmHg·ml⁻¹·s⁻¹). *Significant difference from the baseline values, P < 0.05. †Significant difference between the 2 groups, P < 0.05.

References

1. ** Relationship between the HF/Total component and HR.** To evaluate the relative contribution of cardiac sympathetic and parasympathetic outflows to autonomic control of HR in the intact condition, the relationship between the relative changes in the HF/Total component (as an index of CVNA) and HR are compared between normal and tetraplegic subjects in scattered diagrams of Fig. 5. The slope of the gross linear relationship between the changes in the HF/Total component and HR...
during exercise was steeper in the normal group than in the tetraplegic group; the linear regression line was $y = -0.34x + 33.81$ for the normal group and $y = -0.28x + 27.64$ for the tetraplegic group. At the start of static exercise, HR was more shifted upward in normal than tetraplegic subjects, despite the same initial decrease in the HF/Total component (Fig. 5). Because the HF/Total component decreased during static exercise, HR increased in both groups. It is noted that, because the peak decrease in the HF/Total component at the end of exercise was greater in tetraplegic than normal subjects, the increase in HR reached the comparable level compared with normal subjects. Immediately after the end of exercise, a quick reduction in HR was followed by a gradual recovery in the HF/Total component in normal subjects (Figs. 3 and 5). On the other hand, in tetraplegic subjects, the increase in HR tended to diminish in parallel with a gradual recovery in the HF/Total component.

**DISCUSSION**

Tetraplegic persons are deprived of supraspinal sympathoadrenal control but have intact vagal efferent pathway. In addition, circulating plasma epinephrine and norepinephrine do not increase during sustained contraction of elbow flexor muscles in tetraplegic subjects (41). In humans with tetraplegia, consequently the autonomic control of HR during voluntary static arm exercise is accomplished by cardiac parasympathetic outflow only. The changes in the HF component of HRV are...
sympathetic decentralization causes the decreased capacity to the rapid adaptation of HR, especially at the start of exercise and immediately after the end of exercise.

Baseline HR variability in tetraplegic subjects. It has been thought that the HF component in the power spectrum of HRV mainly reflects cardiac parasympathetic outflow, whereas the LF component may reflect cardiac sympathetic outflow but have a complicated relation with cardiac parasympathetic outflow (33). If so, it is expected that the resting HF component will not be changed in humans with tetraplegia and the resting LF component will be reduced. In this study, the absolute values of the HF and LF components in tetraplegic subjects were not different from those in normal subjects, although they tended to be exaggerated. The augmented HF component with tetraplegia may suggest a long-term adaptive change in cardiac parasympathetic outflow following spinal cord injury. Another suggestion is that because the HRV, including the LF component in tetraplegic subjects, is produced by cardiac parasympathetic outflow only, the LF component is not a reliable measure as cardiac sympathetic outflow and is strongly affected by cardiac parasympathetic outflow as well. This is supported by previous studies (1, 15) demonstrating that the LF component of HRV is significantly reduced after vagal blockade.

HR variability during static exercise in tetraplegic subjects. When a conventional power spectrum analysis of HRV, such as a Fourier transform analysis, has been applied to examine the HF component during head-up tilt in tetraplegic subjects, the HF component showed an abnormal response (9, 10) or the similar response as normal subjects (8, 11). One reason responsible for the contradictory results is that the Fourier spectral analysis is not appropriate to evaluate the dynamic change in HRV during head-up tilt because of limitations inherent in the stationary hypothesis (33). A wavelet transform analysis of HRV, which allows a temporally localized sliding analysis of the signal to access the status of HRV at any time, will be useful to identify the instantaneous changes in cardiac parasympathetic outflow during voluntary behavior. Thus we attempted to identify cardiac parasympathetic outflow from HRV during voluntary static arm exercise using the wavelet transform power spectrum analysis. The decrease in HF/Total power in tetraplegic subjects tended to be greater than that in normal subjects during the later period of exercise, whereas the increase in HR was the same between both groups (Figs. 4 and 5). Because CSNA abruptly increased at the onset of exercise and remained elevated throughout the exercise in cats (36), the increase in HR in normal subjects was mediated by both sympathetic activation and vagal withdrawal. Therefore, the present results suggest that an augmentation of cardiac vagal withdrawal might occur in tetraplegic subjects devoid of central sympathetic control to increase in HR to similar level as in normal subjects.

On the other hand, the LF component of HRV may reflect some form of sympathetic modulation and have a more complex relation with cardiac autonomic nervous activity (33). The LF and LF/Total components tended to increase during static exercise in normal subjects, whereas they decreased in tetraplegic subjects (Fig. 4). This difference should be attributed to the effect of cardiac sympathetic decentralization. Previous studies investigating the LF component in tetraplegic subjects demonstrated that the LF component might be mediated by spinal
sympathetic circuit (9, 10, 14). However, the present finding that the decreases in the LF and LF/Total components were in parallel with the reduction in the HF/Total component in tetraplegic subjects implies a role of cardiac parasympathetic outflow as a cause of the LF component. Therefore, our findings refute the notion that the LF component, both in absolute units and in units divided by total power, reflects only cardiac sympathetic nerve traffic to the heart. The present findings suggest important implications for clinical and experimental estimation of cardiac sympathetic nervous activity.

Neural mechanisms for the tachycardia at the onset of static exercise. It has been generally considered that an instantaneous acceleration of HR during voluntary exercise is predominantly caused by cardiac vagal withdrawal but not by stimulation of cardiac sympathetic outflow (26, 27). This assumption has been partly based on the evidence derived from the delayed response in muscle sympathetic nerve activity (MSNA) during exercise (17, 37, 38). However, it is fundamentally difficult to extrapolate CSNA from the data of MSNA, because the sympathetic nervous system possesses a widespread regional difference. A role of cardiac sympathetic outflow in regulation of HR during exercise has also been indirectly estimated from the effect of \textsuperscript{-}adrenergic and/or muscarinic blockade on the exercise-induced tachycardia (26). However, the autonomic blockade alters baseline HR itself, which in turn can modify the response in HR during exercise and cardiac autonomic outflow. From these reasons, we believe that the data of MSNA and the effect of autonomic blockade on the tachycardia are limited in estimating the response in cardiac sympathetic outflow during exercise. Although cardiac norepinephrine spillover is a more reliable estimate for CSNA, it lacks high time resolution and requires invasive treatment. In contradiction to the conventional thought, we recently hypothesized that abrupt stimulation of CSNA played an important role in rapidly accelerating HR at the start of exercise and cardiac sympathetic decentralization precluded the rapid increase in HR at the onset of exercise, because the increase in HR at the onset of voluntary static arm exercise was blunted in tetraplegic subjects compared with age-matched normal subjects (31). However, as another possibility, it could not be excluded that a blunted response of CVNA, in association with loss of supraspinal sympathetic control, may limit the initial tachycardia. Considering that the HF and HF/Total components similarly decreased at the start of static exercise in both normal and tetraplegic subjects, cardiac vagal withdrawal during static exercise in tetraplegic subjects is comparable to healthy normal subjects. Therefore, the attenuated response in HR at the initial period of exercise in tetraplegic subjects is attributed to the effect of cardiac sympathetic decentralization. In other words, CSNA plays an important role in the rapid acceleration of HR at the onset of exercise, in concert with a gradual reduction in CVNA. In agreement with this conclusion, our laboratory has recently found that an abrupt increase in CSNA preceded the initial tachycardia at the onset of dynamic exercise in conscious cats (36).

Recovery process of HR following exercise. Regarding the autonomic control of the HR recovery following exercise, it is generally considered that the HR recovery after exercise is
predominantly mediated by restoration of CVNA but not a concomitant reduction in increased CSNA, because the HR recovery was prolonged by parasympathetic blockade (7, 12, 28) but was unaffected by sympathetic blockade (4, 12, 28). If this view is true, the recovery of HR immediately after exercise in tetraplegic subjects with intact vagal efferent pathway will be expected to have the same characteristics as normal subjects. However, we revealed that HR in tetraplegic subjects decreased more slowly to the preexercise level following the end of exercise compared with normal subjects (Fig. 2). On the other hand, the HF/Total component was gradually restored with the same time course in both groups, indicating that cardiac vagal restoration in tetraplegic subjects is comparable to normal subjects (Figs. 3 and 5). Plasma epinephrine and norepinephrine did not raise at all during static exercise in humans with tetraplegia (41). Therefore, the delayed HR recovery in tetraplegic subjects after exercise is produced by a gradual restoration of CVNA but not by a reduction in circulating catecholamines. In other words, it is likely that a rapid reduction in CSNA contributes to the HR recovery in concert with a gradual restoration of CVNA. This hypothesis is supported by our laboratory’s recent evidence that when cardiac sympathetic efferent discharge was measured during treadmill exercise in conscious cats, CSNA returned promptly to the preexercise level within 1 s immediately after the end of exercise (36). On the other hand, because the rise in MAP at the end of exercise was much greater in normal subjects than tetraplegic subjects, arterial baroreceptors will be more stimulated in normal subjects, which elicits baroreflex vagal bradycardia following exercise. The present result that the HF component tended to increase transiently above the preexercise control level following exercise in normal subjects may reflect an enhancement of cardiac vagal outflow due to arterial baroreflex, which in turn may partly contribute to the faster recovery of HR in normal subjects.

**Limitations.** Several limitations are involved in this study. First of all, the sample size involved in this study, especially the number of the tetraplegic subjects, may not be large enough to draw a definitive conclusion. Although the small sample size may partly explain large interindividual variation in the power spectral data of HRV, we found the significant decreases in the HF and HF/Total components from the baseline control during static exercise. Second, it is known that the HF component of HRV does not accurately reflect CVNA if respiratory frequency and/or tidal volume changes during an experimental intervention. An increased tidal volume enhances the HF power, whereas an increased respiratory frequency diminishes the HF power (2). Because we instructed the subjects to breathe naturally without any respiratory intervention, the reduction in the HF component obtained in this study might be secondary to decreasing tidal volume and/or increasing respiratory frequency rather than cardiac vagal withdrawal. Indeed,
Taylor et al. (35) have recently shown that the respiratory pattern, including respiratory frequency and tidal volume, is similar in tetraplegic and normal subjects. The increase in minute ventilation and tidal volume is greater than the minute ventilation required during static arm exercise (19). However, Iellamo et al. (11) have shown that the respiratory frequency at rest and during head-up tilting are not statistically different between tetraplegic and normal subjects. During static arm exercise, in normal subjects minute ventilation increased ~7–13 l/min during static handgrip of 30% MVC (6). The same increase in minute ventilation will be expected during static arm exercise in tetraplegic subjects. The maximum minute ventilation tested during arm dynamic exercise reached ~50 l/min in tetraplegic subjects (3), which is much greater than the minute ventilation required during static exercise of 30% MVC. Thus we believe that the respiratory changes exert a minimal effect in the present study, even if tetraplegic subjects have an impairment of lung function (19). However, the measurement of respiratory pattern, including respiratory rate and tidal volume during static exercise, in tetraplegic subjects will be needed in a future study. Third, Taylor et al. (35) have recently shown that β-adrenergic blockade enhanced respiratory sinus arrhythmia, suggesting that respiratory sinus arrhythmia is not simply modulated by cardiac parasympathetic outflow but also by cardiac sympathetic outflow. If so, the baseline values of the HF and HF/ Total components and their responses to static arm exercise might be influenced by cervical spinal cord injury with sympathetic decentralization. However, the baseline of the HF component and its responses to static exercise were not different between tetraplegic and normal subjects. Judging from these results, we must say that the HF components mainly reflect cardiac vagal outflow with a minimal effect of cardiac sympathetic activity and that cardiac vagal outflow is similar between both groups. However, a possibility that a long-term adaptive change in cardiac vagal outflow following spinal cord injury may affect the present results cannot be excluded. Finally, Nakamoto et al. (21, 22) have recently shown that when HR reaches 90–100 beats/min during dynamic exercise, the variability of R-R interval is dissociated from the variability of P-P interval and becomes much smaller than that of P-P interval. This finding has suggested for the first time that the power spectral analysis of R-R interval variability during exercise could not reflect cardiac autonomic nervous activity to the sinoatrial node if HR increases beyond 90–100 beats/min. However, because the maximal HR during static exercise in this study was below that HR level, the HF power and HF/ Total components obtained from the R-R interval variability reflect those obtained from the P-P interval variability.

In conclusion, although cardiac parasympathetic outflow in humans with tetraplegia responds to voluntary static exercise similarly as healthy normal subjects, the acceleration of HR at the start of exercise and the deceleration of HR following exercise are impaired. Thus sympathetic decentralization causes the decreased capacity to the rapid adaptation of HR in association with voluntary exercise.

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